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- **1** A novel microfluidic device capable of maintaining functional thyroid carcinoma
- 2 specimens *ex vivo* provides a new drug screening platform.
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21 Abstract

22 Background: Though the management of malignancies has improved vastly in recent 23 years, many treatment options lack the desired efficacy and fail to adequately 24 augment patient morbidity and mortality. It is increasingly clear that patient response 25 to therapy is unique to each individual, necessitating personalised, or 'precision' 26 medical care. This demand extends to thyroid cancer; ~10% patients fail to respond to radioiodine treatment due to loss of phenotypic differentiation, exposing the patient to 27 28 unnecessary ionising radiation, as well as delaying treatment with alternative 29 therapies.

30 Methods: Human thyroid tissue (n=23, malignant and benign) was live-sliced (5mm 31 diameter x 350-500µm thickness) then analysed or incorporated into a microfluidic 32 culture device for 96hr (37°C). Successful maintenance of tissue was verified by 33 histological (H&E), flow cytometric propidium iodide or trypan blue uptake, 34 immunohistochemical (Ki67 detection/ BrdU incorporation) and functional analysis 35 (thyroxine [T4] output) in addition to analysis of culture effluent for the cell death 36 markers lactate dehydrogenase (LDH) and dead-cell protease (DCP). Apoptosis was investigated by Terminal deoxynucleotidyl transferase dUTP nick end labelling 37 38 (TUNEL). Differentiation was assessed by evaluation of thyroid transcription factor 39 (TTF1) and sodium iodide symporter (NIS) expression (western blotting).

40 *Results:* Maintenance of gross tissue architecture was observed. Analysis of 41 dissociated primary thyroid cells using flow cytometry both prior to and post culture 42 demonstrated no significant change in the proportion of viable cells. LDH and DCP 43 release from on-chip thyroid tissue indicated that after an initial raised level of release, 44 signifying cellular damage, detectable levels dropped markedly. A significant increase 45 in apoptosis (*p*<0.01) was observed after tissue was perfused with etoposide and JNK</p>

inhibitor, but not in control tissue incubated for the same time period. No significant
difference in Ki-67 positivity or TTF1/NIS expression was detected between fresh
and post-culture thyroid tissue samples, moreover BrdU positive nuclei indicated onchip cellular proliferation. Cultured thyroid explants were functionally viable as
determined by production of T4 throughout the culture period.

Conclusions: The described microfluidic platform can maintain the viability of
thyroid tissue slices *ex vivo* for a minimum of four days, providing a platform for the
assessment of thyroid tissue radioiodine sensitivity/adjuvant therapies in real time.

Keywords: Thyroid gland, Microfluidics, Viability, De-differentiation, Radioiodine
therapy.

63 Introduction

64 Thyroid carcinoma (TC) is the most common malignant disease of the human endocrine system, accounting for ~2.1% of all cancer cases worldwide, and 65 66 disproportionately affecting women (1). The incidence of TC has increased by 139% since the early 1990's in the United Kingdom, with a particular increase in the 67 68 diagnosis of papillary TC (PTC; Cancer Research UK [2018]). PTC, along with follicular-TC (FTC), form the differentiated TC group (DTC), which represent ~90% 69 70 of all thyroid malignancies (2). Patients with DTC have a 10-year survival rate of 71 90%, underpinned by an efficacious treatment regimen, which includes thyroidectomy followed by remnant and metastatic ablation using radioactive iodine (^{131}I) . 72

Treatment, using ¹³¹I, capitalises on the ability of thyrocytes to absorb iodide 73 74 (Γ) for thyroid hormone biosynthesis. Γ is transported across the basolateral 75 membrane of thyrocytes by the sodium iodide symporter (NIS) using the sodium gradient generated by Na^+/K^+ -ATPase (3). Due to the essential involvement of the 76 77 NIS in thyroid hormone biosynthesis and thus human metabolism in general, 78 expression of the NIS is tightly regulated. In thyroid cancer, thyroid peroxidase (TPO) 79 activity, and thus organification of free iodide is reduced. Oxidised iodine possesses a 80 significantly longer retention time than free iodide, leading to a considerably reduced 81 effective half-life in the malignant compared with the benign thyroid (0.5-3 days vs. 3-7 days, respectively; [4]). Despite this, treatment of DTC using ¹³¹I remains an 82 83 effective means of eradicating remnant and metastatic malignant foci when a high 84 dose can be delivered to the target tissue (5). However, in approximately 15% of DTC cases, basolateral expression of the NIS is lost, due to phenotypic de-differentiation of 85 thyrocytes, rendering ¹³¹I therapy ineffective (6). Within this cohort of patients, the 86 use of ¹³¹I therapy is negated, as thyrocytes cannot concentrate ¹³¹I, leading to a 87

88 marked reduction in patient survival (only 10% alive at 10-years, mean survival 3-5 89 years; [7]). Treatment of advanced, ¹³¹I refractory TC using traditional systemic 90 therapies including doxorubicin has limited efficacy with a high toxicity rate (8). 91 Alternative therapy using relatively new-to-market tyrosine-kinase inhibitors (TKI), particularly sorafenib and lenvatinib, has garnered significant interest and has shown 92 93 objective response rates with significantly improved progression-free survival (9,10). 94 Currently it is not possible to predict accurately a lack of response to ¹³¹I prior to administration, thus patients have a delay before receiving effective adjuvant therapy 95 96 (11). Although it is well accepted that iodide uptake is typically reduced in malignant 97 thyroid tissue relative to surrounding tissue (12), the molecular underpinnings have 98 not yet been fully elucidated. A previous study by Min et al. (6) investigated the relationship between NIS expression and ¹³¹I uptake in recurrent TC using 99 100 immunohistochemical (IHC) analysis. They found that although lesional NIS expression predicted ¹³¹I uptake with 100% specificity, the sensitivity of this method 101 was just 50% (14 of 28 patients with positive ¹³¹I uptake had negative NIS staining. 102 103 Similarly, Arturi et al. (13) found, in a smaller study using RT-PCR, that only 4 out of 8 (50%) primary DTC with distant metastases and negative ¹³¹I uptake lacked NIS 104 105 gene expression in the primary lesion; thus indicating that assessment of NIS expression is certainly not an infallible means of evaluating ¹³¹I uptake. Furthermore, 106 107 Saito et al. (14) unexpectedly detected increased NIS mRNA and protein levels in 108 PTC tissue compared with normal thyroid tissue. This variability suggests that 109 reduced iodide uptake is perhaps due to failure to target or retain NIS protein at the 110 basolateral membrane (15), rather than abrogated NIS protein production.

111 The microfluidic system described herein uses precision cut tissue slices112 (PCTS) which maintain the multicellular 3D architecture of the thyroid tissue

113 essential for intercellular communication, which is not well recapitulated in standard 114 *in vitro* systems. Two previous studies have employed static culture of thyroid tissue 115 explants: Russo *et al.* (16) investigated apoptosis subsequent to 131 I treatment in 116 1mm³ tissue fragments, whereas Nagy *et al.* (17) examined the effect of various 117 hormones and cytokines on the proliferation of 2mm³ thyroid fragments. The results 118 from these studies demonstrated that thyroid tissue cultured *ex vivo* can respond to 119 external stimuli, however clinical utility was not assessed.

120 The bespoke device described in this manuscript mimics the in vivo 121 vasculature and lymphatics by allowing continual perfusion of explanted tissue, along with removal of waste products and allows precise control of drug delivery (18). 122 Future treatment of *ex vivo* thyroid tissue maintained in this device with ¹³¹I, holds 123 potential for a more realistic estimation of ¹³¹I treatment success by assaying not only 124 125 uptake, but resultant cell death. The aim of this study was to characterise a reproducible, easy to use, microfluidic system to maintain precision sliced ex vivo 126 127 thyroid tissue for up to 96hr.

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133 Materials and methods

134 Fabrication of a microfluidic culture device

Two polyether ether ketone plastic plates (PEEK; Direct Plastics, Sheffield, 135 136 UK), both 30mm x 14mm in size (figure 1-A), were milled centrally to produce 137 threaded axial holes to which inlet and outlet ethylene tetrafluoroethylene tubing (ETFE; 0.8mm internal diameter; Kinesis, IDEX Health & Science, Cambridge, UK) 138 139 was attached via coned adapters (LabSmith, Mengel Engineering, Denmark). In addition, four 1/4 inch (6.35mm) holes were made in both PEEK plates to allow the 140 141 insertion of nylon screws in order to secure the unit after sample addition. A central cylindrical recess (10 x 4mm) was drilled in each PEEK plate to house a porous 142 143 sintered pyrex disc (figure 1-A; The Lab Warehouse, Grays, UK). Finally, a silicone gasket (30mm diameter; 1 mm sheet silicone) with a 6mm central hole to create a 144 145 tissue well, was placed between the two PEEK plates.

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Sample collection and preparation

Human thyroid tissue samples (n=23 malignant; n=14 benign) were collected 147 at the point of surgical resection during thyroidectomy following written informed 148 149 consent under ethical approval from North East-Newcastle and North Tyneside 150 Research Ethics Committee (15/NE/0412) and Hull and East Yorkshire NHS Trust 151 R&D (R1925). Benign thyroid tissue was collected alongside malignant tissue when 152 deemed practicable by consultant surgeon JE (n=14). Details of obtained tissue specimens are summarised in Table 1. Tissue samples were transported to the 153 154 laboratory in ice-cold complete medium, then processed, allowing culture initiation 155 within 60 minutes of surgical excision. Tissue was immobilised on a piece of cork and

156	sliced at a thickness of either 350 or $500\mu m$ in ice-cold PBS using a vibratome (Leica
157	VT1200S, Milton Keynes, UK) with a blade speed of 0.1 mm s ⁻¹ and amplitude of
158	2.5mm. A skin biopsy punch (Stiefel, Middlesex, UK) was used to generate PCTS
159	5mm in diameter. Each PCTS was weighed before insertion into the device. Where
160	samples sizes differ across experimental time-points this was due to difficulties in
161	effluent collection, sample numbers collected are provided in figures.

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No	Tumour stage	Patient age	Gender	Tissue received
1	T2NXMX	45	М	М
2	T4aN1bMX	46	F	М
3	T3aNXMX	49	М	М
4	BG	56	М	В
5	T2NXMX	50	F	M,B
6	T3N1bMX	28	F	М
7	T4N0M0	80	F	М
8	T1aNXMX	64	F	М
9	BG	62	F	В
10	T2N1BMX	33	F	M,B
11	T3N1aMX	52	F	М
12	BG	34	F	В
13	BG	51	М	В
14	T4N0M1	51	F	М
15	T1aN1bMX	43	F	М
16	T1bNXMX	49	М	M,B
17	T3aNXMX	19	М	М
18	T3bN1aMX	44	М	M,B
19	T1NXMX	69	F	M,B
20	T1aNXMX	19	М	М
21	T3AN1bMX	32	F	M,B
22	T3aN1bM0	21	F	М
23	T1aNXMX	48	F	M,B
24	T3N1bM0	30	F	M,B
25	T2NXMX	73	F	M,B
26	T3aNXMX	62	F	М
27	T4aN1bMX	73	М	M,B

163 Table 1: Disease and patient characteristics of thyroid specimens used in this study

BG: Benign goitre; **M**: Malignant tissue; **B**: Benign tissue.

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166 PCTS culture set up

167 Dulbecco's modified eagles medium (DMEM; GE Healthcare, Yeovil, Somerset, UK) containing 10% (v/v) heat inactivated foetal bovine serum (FBS; 168 169 Biosera, East Sussex, UK), penicillin/streptomycin (0.1U/ml and 0.1mg/ml 170 respectively; GE healthcare), 0.4mM glutamine (GE healthcare) and 2.5µg/ml 171 Amphotericin B (Life Technologies, Paisley, UK) was supplemented with thyrotropin [TSH; 2 mIU/L (normal serum 0.3–5 mIU/L)] and sodium iodide (0.1µg/ml). 172 173 'Complete medium' was then loaded into a 20ml syringe and connected to the 2-part 174 adapter and ETFE tubing via a 0.22µm filter (Figure 1; Millipore, Watford, UK). The 175 PCTS was loaded onto a 70µm nylon porous membrane placed on top of the sintered disc in the inlet PEEK plate, and the outlet PEEK plate was then secured in place 176 177 using nylon screws. The syringe was connected to a Harvard PhD 2000 syringe pump 178 (Harvard, Cambridge, UK), which provided a pressure driven perfusion rate of 2µl min⁻¹. The culture device was maintained at 37°C inside an incubator for 96hr. Media 179 180 coming off the chip was collected in 1.5ml polypropylene tubes after 2hr culture, then 181 in 15ml polypropylene tubes once per day thereafter. Where required, for proliferation analyses, the thymidine analogue Bromodeoxyuridine (BrdU; Sigma-Aldrich, 182 183 Gillingham, UK) was added, at 10µM final concentration, to the complete medium for 184 the final 24 hours of culture (19).

185 Tissue embedding and morphological analysis

Fresh and post-culture tissue samples were either frozen in Tissue-Tek OCT (optimum cutting temperature; Sakura, Berkshire, UK) medium, using liquid nitrogen-cooled 2-methylbutane (Sigma-Aldrich), or fixed in 4% paraformaldehyde

(PFA) for 24hr. PFA fixed tissues were then dehydrated through an ethanol gradient
(70, 90, 95, 100%), incubated with two changes of molten paraffin wax, then
embedded and allowed to cool. Frozen tissue sections were cut at a thickness of 8µm
using a Leica CM1100 cryostat and fixed for 20 minutes in -20°C cooled methanol
before standard staining using Haematoxylin and Eosin (H&E; [20]). PFA fixed,
paraffin embedded (PFPE) tissues were sectioned using a Leica RM2135 microtome
(5µm).

196 Measurement of lactate dehydrogenase release

197 Lactate dehydrogenase (LDH) is a cytosolic enzyme released from the cell 198 after plasma membrane damage (21). As membrane damage is synonymous with cell 199 death, its release allows monitoring of the loss of cell viability (Cytotoxicity 200 Detection Kit Plus, Roche, UK). Culture effluent (n=14 malignant, n=10 benign 201 patient samples) was collected daily and stored at 4°C until the end of the culture 202 period (96hr). In some cases (n=7) tissue was removed from the culture system at the 203 end of the 96hr incubation and exposed to a 10% (v/v) lysis buffer overnight to induce 204 cell death and subsequent LDH release. The assay was conducted following the 205 manufacturer's protocol and results expressed as an average of duplicate readings 206 normalised per mg of thyroid tissue.

207 Measurement of protease release

The CytoTox-Glo[™] Cytotoxicity Assay (Promega, Southampton, UK) allows
measurement of cell death using a luminogenic peptide substrate (alanylalanylphenylalanyl-aminoluciferin; AAF-Glo[™] Substrate) to measure the activity of
proteases released from non-viable cells that have lost membrane integrity. Culture
effluent samples (including positive controls exposed to 10% (v/v) lysis buffer; 100µl

per well) were added in duplicate to a 96-well white-walled microplate. Malignant tissue samples were prioritised for use in DCP analysis. Assay Reagent (50µl) was then added to all wells and mixed briefly by orbital shaking. The reaction was incubated at room temperature for 15 minutes, before luminescence was measured using a Victor multilabel plate reader according to the supplier's protocol (n=7; PerkinElmer, Coventry, UK).

219 Viability analysis of dissociated cells

Malignant thyroid tissue was dissociated into a single cell suspension (n=3)220 221 prior to and after maintenance on the device by initial mincing using scalpels 222 followed by a 2hr incubation (37°C; 5% CO₂) with 0.024% (w/v) Collagenase IV 223 (Sigma-Aldrich: Dorset, UK) and 0.02% (w/v) DNase I (Roche, Herefordshire, UK) 224 in complete medium under constant rotation. The resultant suspension was passed 225 through a 70µm filter (BD Biosciences, Oxford, UK) prior to centrifugation at 400 x g 226 for 5 minutes, to pellet the cells. The cell pellet was resuspended in 1ml of complete 227 medium before viability was quantified using trypan blue exclusion. The cells were 228 rinsed in PBS (Oxoid, Thermo Scientific, Hampshire, UK)/ BSA (2.5g/L; Thermo 229 Scientific, Loughborough, UK)/Azide (0.0624% [v/v]; Sigma-Aldrich) and dead cells 230 were stained by the addition of propidium iodide (500µg ml⁻¹). Cells were acquired 231 immediately using a FACS Calibur flow cytometer (BD Biosciences) alongside unstained cells as a reference and results were analysed using Cell Quest Pro software, 232 version 6.0. 233

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236 Terminal deoxynucleotidyl transferase-mediated dUTP nick-end labelling 237 (TUNEL) assay

238 Frozen tissue sections were defrosted for 5 minutes prior to fixing in 4% PFA for 20 239 minutes at room temperature. PFPE tissue sections were dewaxed in xylene (20 240 minutes) then rehydrated in 100%, 90% and 70% ethanol (2min per wash). Sections 241 were treated for 20 minutes at 37°C (PFPE tissue) or 2 minutes on ice (frozen tissue) with 0.1% proteinase K/1% TrisHCl in dH₂0. Sections were washed twice with PBS 242 243 for 5 minutes and apoptotic cells were labelled using an In Situ Cell Death Detection 244 Kit (Roche, UK) according to the manufacturer's guidelines. Negative control 245 sections were incubated with 50µl label solution only, whereas test sections were 246 incubated with both the label and enzyme solution. Sections were counterstained using a DAPI-hardset mounting medium (Vector Laboratories, UK) before 247 248 fluorescence was evaluated using an ImageXpress Micro 4 Imaging System 249 (Molecular Devices, California, USA). Produced tiled images were stitched to create a 250 single composite image before apoptotic nuclei were quantified using ImageJ (Fiji 251 plugin (22))

252 Treatment of thyroid tissue with etoposide and SP600125

Thyroid explants were exposed to etoposide and SP600125 for the complete (96hr) culture period in order to examine the ability of the system to induce a response which was then quantifiable using TUNEL staining. Etoposide, a topoisomerase II inhibitor, and SP600125, a JNK inhibitor, were added to complete culture medium at a concentration of 20μ M, then perfused through the culture system under the same conditions as control samples.

260 Immunohistochemical analyses

261 Frozen tissue sections (8µm) were fixed in pre-cooled (-20°C) acetone for 20 minutes. Frozen tissue sections to be stained with anti-BrdU primary antibody were 262 transferred into 2M HCl for 30min to denature the DNA and allow access of the 263 264 antibody to the incorporated BrdU before being neutralised in borate buffer (0.2M 265 boric acid, 0.05M sodium tetraborate [pH 8.4]; 2 x 5 min washes). PFPE tissue sections were dewaxed and rehydrated as previously described. Endogenous 266 267 peroxidases were blocked in 3% (v/v) H₂O₂ (Fisher Scientific, Loughborough, UK) in acetone for 15 minutes. Antigen retrieval was carried out on paraffin embedded tissue 268 269 sections by microwave boiling within Antigen Unmasking Solution (citrate based; pH 270 6.0, Vector Laboratories, Peterborough, UK) for 20 minutes. Slides were loaded into SequenzaTM racks and sections were incubated with normal horse blocking serum 271 (Vectastain Elite ABC kit, Vector Laboratories) for 20 minutes. The addition of 272 273 avidin D solution and, after a TBS wash, biotin solution (Vector Laboratories) for 15 274 minutes blocked non-specific binding of the avidin/biotin system.

275 Sections were incubated with primary antibody or matched isotype control 276 antibody overnight at 4°C [Ki67 clone MIB1, 1:100 (Dako, Agilent, Stockport, UK)]; [BrdU clone 3D4, 1:50 (BD Biosciences)]; [TTF1 clone EP1584Y, 1:250 (AbCam)]. 277 278 Following a TBS wash sections were incubated with secondary antibody (Vectastain 279 Elite ABC kit) for 30 minutes followed by ABC detection reagent for 30 minutes. 280 Colour was developed using 3,3'-diaminobenzidine (DAB; Sigma-Aldrich) and 281 sections counterstained with Harris Haematoxylin. Sections were dehydrated and 282 cleared through graded alcohols and histoclearTM (Scientific laboratory supplies, Nottingham, UK) then mounted using histomount (Scientific laboratory supplies). 283

The percentage of DAB positive cells was assessed across five separate fields using
the online applet Immunoratio (http://153.1.200.58:8080/immunoratio/; (23)).

286 Assessment of NIS protein expression by Western blotting

287 Both fresh and post-culture thyroid tissue samples were minced using scalpel blades in ice cold RIPA buffer (Sigma-Aldrich) containing 1% (v/v) protease 288 289 inhibitors (Roche) and sonicated for 1 minute before being agitated using a 290 MACSmix[™] tube rotator (2hr, 4°C; Miltenyi Biotec, Surrey, UK). Samples were then centrifuged at 16,000 x g for 20 minutes at 4°C, before the supernatant was aliquoted 291 292 and frozen (-80°C). Proteins were quantified using a PierceTM BCA Protein Assay Kit 293 (Thermo Scientific) then 10µg was resolved on a 4% (v/v) stacking, 12% (v/v) 294 separating sodium dodecyl sulfate-polyacrylamide gel in a Mini-PROTEAN® system, 295 before being transferred onto nitrocellulose membranes using a Trans-Blot Turbo[™] 296 (both Bio-Rad, Watford, UK) and blocked in 4% bovine serum albumin (BSA) in 297 TBS-Tween overnight. NIS was detected using a rabbit anti-human polyclonal 298 antibody (ab199410, Abcam, Cambridge, UK) diluted 1:500. The house keeping gene 299 β -actin was detected using a mouse anti-human antibody (sc-516102, Santa-Cruz 300 Biotechnology, Heidelberg, Germany) diluted 1:10,000. Blots were developed using 301 SuperSignal[™] West Pico PLUS Chemiluminescent Substrate (Thermo Scientific) and 302 Radiomat LS film (Agfa Healthcare, Middlesex, UK). Densitometry of bands was 303 analysed using a Gel Doc system (Bio-Rad).

304 Measurement of thyroxine release by ELISA

Thyroxine (T4) is the principal hormone released by the thyroid gland, thus, its release from on-chip thyroid tissue was investigated using an enzyme-linked immunosorbent assay (ELISA, Abcam), according to the manufacturer's instructions,

308 as a measure of *ex vivo* functionality. Briefly, effluent samples (n=7 malignant, n=7 309 benign), controls and standards (25µl) were loaded in duplicate into a pre-coated 96 310 well plate, followed by 100µl working concentration of conjugate reagent. The plate 311 was incubated for 60 minutes at room temperature. Each well was washed 5 times 312 with distilled water before TMB (3,3',5,5'-Tetramethylbenzidine; 100µl) reagent was 313 added before a further 20-minute incubation. The reaction was stopped by the 314 addition of 100µl stop solution (2N Sulphuric acid [H₂SO₄] VWR, Leicestershire, UK) 315 to each well. Absorbance was measured at 450nm using a Multiskan plate reader 316 (Thermo Scientific). T4 concentration in each sample was determined from the 317 standard curve and normalised per mg of thyroid tissue.

318 Results

The morphology of both freshly resected and post-culture (96hr) *ex vivo* thyroid tissue sections was assessed by H&E staining and showed preservation of gross morphology, with retention of tissue cohesion (figure 2). The follicular structure, typical of *in vivo* thyroid tissue, was clearly displayed in both fresh and post-culture tissue samples. Inter-tumour variation in cellularity and follicle size is clear, however these differences are retained in tumour tissue throughout culture.

Culture effluent was sampled throughout the 96hr culture period and examined for the presence of two markers of cell death, LDH and DCP. An initial raised level of LDH release was observed within the first 2hr of culture setup (figure 3A), which reduced after 24hr and remained consistently low for the remaining 72hr, until tissue was exposed to 10% (v/v) lysis buffer, which led to an average increase in LDH release from 0.01 \pm 0.002 to 0.304 \pm 0.06 and 0.005 \pm 0.001 to 0.35 \pm 0.03 absorbance units mg⁻¹ in malignant and benign thyroid tissue, respectively. No difference in LDH release was found between the malignant and the benign tissue. DCP release by cells in the culture system followed a profile similar to that of LDH release (figure 3B), with the level being relatively high in the first 2hr of culture before decreasing after 24hr. DCP release reached a minimum after 72hr, with only 41.53 ± 28.33 RLU mg⁻¹ detectable. Concordant with LDH release, purposeful lysis of cultured thyroid tissue subsequent to 96hr culture induced a >1000-fold increase in detectable DCP.

No significant difference in viability between fresh (27.3 ±7.3%) and post-338 339 96hr cultured (24.6 ±8.8%) malignant thyroid tissue samples was observed using PI 340 staining to (Figure 4; n=3; p=0.19). These data were consistent with results using 341 trypan blue exclusion to represent cell viability, whereby the mean proportion of 342 viable dissociated cells was $38.33 \pm 7.3\%$ in fresh thyroid tissue prior to culture and 34 $\pm 9.5\%$ in tissue after a 96hr culture period (figure 4; n=3; p=0.37). The proportion of 343 344 apoptotic cells in both fresh and post-culture (+96hr) malignant thyroid tissues was 345 assessed by TUNEL staining (n=9) and a small, non-significant, increase in apoptotic 346 cells was observed in the post-culture tissue (5.59±0.99%) compared with the fresh 347 tissue (2.77±0.89%; figure 4-C and D). Moreover, on-chip treatment of thyroid explants with etoposide (topoisomerase II inhibitor) and SP600125 (JNK inhibitor) 348 caused a significant increase in cellular apoptosis after 96hr treatment, compared to 349 350 untreated thyroid tissue (15.25% and 14.24% vs. 5.59%; p=0.0025 and p=0.0069respectively; figure 4). 351

Cell proliferation within the thyroid tumour tissue was investigated by IHC. Two markers were used; Ki67, a nuclear protein expressed during all active phases of the cell cycle (non-senescent cells) and BrdU which is incorporated during s-phase of the cell cycle (24). This analysis demonstrated that proliferating cells were detectable in both freshly resected tissue and post-culture tissue. The mean percentage of Ki-67 357 positive nuclei was 1.45±0.33% and 1.32±0.34% in fresh and post-culture tissue (n=8), respectively; no significant difference in the quantity of proliferating cells 358 359 between fresh and post-culture malignant thyroid tissue was observed (p=0.32). BrdU, 360 which was perfused through the culture system for the final 24hr culture on the device, was clearly visible as incorporated into the cell nuclei of proliferating cells post-361 362 culture, illustrating that on-chip cell proliferation was occurring (figure 5). Subsequent to a 24hr perfusion with 10µM BrdU, 12.09±4.38% cells stained positive 363 364 for BrdU incorporation (n=3). Thyroid transcription factor 1 (TTF1) is crucial for thyroidal organogenesis and differentiation which, along with two other factors, 365 paired box gene 8 (PAX8) and TTF2 (FOXE1), governs the expression of 366 367 thyroglobulin (TG), thyroperoxidase (TPO) and NIS (25). The expression of TTF1 368 was characterised in fresh (0h) and post-culture (+96hr) malignant thyroid tissue; the 369 staining pattern of TTF1 was maintained throughout culture in the microfluidic device (figure 5). 370

371 As expression of the NIS is crucial for adequate response to treatment to I^{131} , 372 it was important to ensure that 96hr culture of malignant thyroid explants within our 373 MF device did not affect NIS protein levels. NIS expression was investigated in both 374 freshly resected and post-culture malignant thyroid tissue and showed that there was 375 no statistically significant difference between the density of NIS protein bands in 376 fresh and cultured thyroid tissue, normalised to β -actin (figure 6; n=5), indicating that 377 the expression of NIS was maintained throughout culture.

The functionality of cultured *ex vivo* thyroid tissue was investigated by its capability to synthesise and release the primary thyroid hormone, T4. Production of T4 occurs as a result of a cycle of biochemical reactions occurring exclusively within the thyroid. Culture effluent was analysed by ELISA for the presence of T4 (n=7 malignant tissue; n=7 benign tissue). Data indicate that T4 release by both malignant and benign thyroid explants follows a similar overall trend, with an initially raised level of T4 production over the first 24hr, stabilising after 48hr (figure 7). Interestingly, T4 release by benign thyroid explants was consistently higher at each timepoint in comparison to malignant tissue and average T4 output throughout the complete culture period was significantly higher in benign tissue (0.29±0.09 µg/dl mg⁻¹) than in malignant tissue (0.14±0.03 µg/dl mg⁻¹; figure 7; *p*=<0.05).

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391 Discussion

392 The current study aimed to characterise the ability of a PCTS device to maintain viable thyroid tissue explants over a 96hr period with a view towards 393 394 therapeutic interrogation. Human tissue explants from human head and neck tumours, 395 intestine and mouse brain have been maintained using similar microfluidic culture 396 systems (20,26,27) however this is, to the best of the authors' knowledge, the first 397 time ex vivo human thyroid tissue has been cultured in a robust, easy-to-use, platform. 398 Tissue sections taken from both fresh and PCTS-cultured thyroid tissue analysed by haematoxylin and eosin and IHC staining demonstrated that morphology was 399 400 preserved in tissue which had been cultured in the device for 96hr, validated by a 401 consultant histopathologist. Results observed agree with those shown in similar 402 studies from the group, whereby head and neck squamous cell carcinoma and full 403 thickness intestinal tissue also demonstrated a preservation of tissue morphology after 404 72hr on-chip culture (18, 20). The gross inter-patient morphology of tissue specimens 405 was variable, and heterogeneity was visible within each tissue sample. Areas of 406 typical thyroidal histology exhibiting follicular architecture often neighboured regions 407 of densely arranged cells or fibrous stroma. This inter- and intra- patient heterogeneity 408 was expected and was also presented in a study by Radu *et al.* (28), who speculated 409 that the morphological variation in thyroid carcinoma is due to manifestation of 410 diverse tumour cell clones under the influence of the same etio-pathogenic factors. It 411 will therefore be necessary to run multiple PCTS chips from the same patient when 412 interrogating the tissue with different treatment regimens.

413 The release of both LDH and DCP as markers of cell membrane integrity was 414 assayed throughout the culture period; loss of cellular plasma membrane integrity is 415 synonymous with loss of cellular viability (29) and microfluidic culture offers a 416 unique means of evaluating this in real time. As anticipated, the release of these two markers followed similar patterns, with a higher level at the beginning of the culture 417 period, attributed to the damage caused to the tissue during preparation, which 418 419 decreased during the remainder of the experiment. The relatively low LDH/ DCP 420 release once the tissue had recovered from the initial cellular damage during set-up, 421 which has also been experienced in previous studies (30,31), indicates cultured 422 explants do not undergo further degradation due to factors such as sheer stress or lack 423 of oxygen within the culture chamber. Deliberate lysis of cultured tissue resulted in an 424 increase in both LDH and DCP, suggesting that a significant number of viable cells 425 remain after 96hr in the PCTS device, which agrees with the morphological 426 assessment. A similar pattern has been observed studies from other groups where 427 stabilisation of LDH release was seen after four days in a four-organ-chip model (32) 428 and after six days in Wagner et al.'s liver/skin co-culture (33). The discrepancy in 429 time taken for tissue to recover from the initial damage could potentially be

430 attributable to either the difference in tissue type, the system used or the presence of431 malignancy in the current system.

Tissue dissociation using a combined mechanical and enzymatic method 432 433 offered an alternative means of investigating the survival of individual cells 434 constituting the gross thyroid explants, by monitoring the ability of propidium iodide and trypan blue to traverse the cellular membrane. Again, no statistically significant 435 436 difference in mean cellular viability was observed between samples which had been 437 dispersed prior to, or after PCTS-culture, further demonstrating that on-chip 438 maintenance was not causing increased cell death. This was despite the fact that the 439 overall viability of cells after dispersal from gross tumour material was unexpectedly 440 low (<40%), presumably due to injury caused by the enzymatic (collagenase IV, DNase II) and mechanical (mincing of gross tissue using scalpel blades) process of 441 442 dissociation. The high level of cell death observed in the current study is in contrast to 443 Li et al. (34) who provided a mean cell viability of 65.66% (±4.96) using trypan blue 444 staining following disaggregation of murine pancreatic fragments using collagenase 445 IV. As malignant tumour tissue is marked by regions of necrosis owing to rapid 446 oncogene-driven proliferation not supported by an adequate vascular bed (35), it is a possibility that presence of necrotic cells contributed to the lower overall viability in 447 448 the current study. The viability of cells dispersed from human head and neck cancer specimens was assessed by flow cytometry in a separate study and produced 449 450 viabilities ranging from 24-92% (36), partially aligning with the results seen here.

To further characterise on-chip tissue kinetics, the proportion of thyroid cells undergoing apoptosis was elucidated through the labelling of 3-OH termini of DNA strand breaks *in situ*, produced due to endonuclease mediated DNA fragmentation, characteristic of DNA degradation and late-stage apoptosis (37). The culture of

455 thyroid explants within the microfluidic device showed no change in the proportion of apoptotic cells. Similar studies have, however, reported comparable levels of 456 457 apoptosis in untreated specimens' post-microfluidic culture. Cheah et al. (22), found 458 an apoptotic fraction of <10% within untreated head and neck squamous cell 459 carcinoma (HNSCC), whilst Wang et al. (38) also saw <10% apoptosis post-culture in 460 brain organoids, compared to ~40% apoptosis in organoids subjected to static culture 461 conditions. The increase in apoptosis observed in this study was not mirrored in other 462 tests of viability such as PI/TB uptake and LDH/DCP leakage data as the latter assays 463 rely on loss of membrane integrity, synonymous with necrotic cell death (38), to facilitate detection of leaked cellular components (LDH/DCP) or PI/TB labelled cells. 464 465 It is feasible that, if cultured for an extended period of time, a decrease in cell viability 466 would also be observed using PI/TB uptake and LDH/DCP leakage assays, due to the 467 occurrence of cell death by alternative mechanisms such as secondary necrosis, 468 characterised by progressive loss of plasma membrane integrity, through caspase-3-469 dependent cleavage of the GSDMD-like protein DFNA5 (38,39). Furthermore, on-470 chip treatment of thyroid explants with 20µM etoposide and SP600125 demonstrates 471 the devices' utility as a drug screening system. Perfusion of thyroid explants with 472 either agent for 96hr resulted in significantly increased levels of apoptosis as examined by TUNEL staining. Etoposide is a well-characterised inducer of apoptosis 473 474 (40) whilst SP600125 is a multikinase inhibitor which has been shown to have both anti-proliferative and migratory effects in thyroid cell lines (41). 475

476 IHC analysis was used to investigate the ability of the cells within the cultured 477 tissue to proliferate. The Ki67 antigen is present in all active stages of the cell cycle, 478 except for $G_{0,}$ in which cells are in a quiescent state (42). Previous studies have 479 attempted to use Ki67 labelling index to aid diagnosis in thyroid neoplasms, however it has shown little value in this setting due to the low labelling index in most thyroid lesions (<1% in 57% PTC samples tested; [43]). In agreement, Ki67-positive brown stained cells were detectable at low levels (<2%) in tissue sections in the current study after 96hr within the PCTS device indicating the presence of a small number of proliferating cells. Furthermore, comparison of the proliferating cell population in both fresh and post-culture thyroid tissue revealed no significant difference.

BrdU staining was also employed, having the added advantage of 486 487 demonstrating definitive on-chip division as BrdU is incorporated into de novo DNA during the S-phase of the cell cycle as a substitute for thymidine and is detectable by 488 IHC (44). Cells with BrdU positive nuclei (12.09%) were evident in thyroid tissue 489 490 samples which had been maintained for 96hr in the PCTS-culture device, the final 24hr of which included perfusion with 10µM BrdU. Identification of BrdU-positive 491 cells throughout the tissue both demonstrates the ability of BrdU to perfuse 492 493 successfully through the tissue and moreover the presence of proliferating cells in the 494 S-phase of the cell cycle. A comparable study by Sart et al. (45) investigated BrdU 495 uptake in H4-II-EC3 rat hepatoma cells cultivated in both a 2D and 3D spheroid setting. The authors saw a near 2-fold decrease in BrdU positivity in 3D (~16%) 496 versus 2D (~30%), similar to results observed in this study. 497

In addition to the viability of the tissue, it was important to characterise the differentiation of thyroid explants, in order to examine whether culture within the microfluidic device could affect the expression of certain genes crucial for successful treatment with radioiodine. A previous study conducted by Cirello *et al.* (46) which aimed to investigate the effects of the multikinase inhibitor SP600125 on multicellular spheroids derived from primary thyroid tissue, examined expression of the transcription factor TTF1 as a marker of differentiation. The authors observed maintenance of TTF1 expression in spheroids derived from primary thyroid tissue.
Encouragingly, the pattern of TTF1 staining in post on-chip culture (+96hr) thyroid
tissue was equivalent to that of fresh thyroid tissue, suggesting that culture for 96hr in
the PCTS device did not markedly affect differentiation.

509 The NIS is an integral plasma membrane glycoprotein that facilitates the accumulation of I⁻ within the thyroid gland at a concentration up to 40 times higher 510 than plasma (47). Application of I^{131} for the targeted destruction of malignant 511 512 thyroidal tissue has become one of the most effective radiation regimens available, 513 causing fewer side effects than other cancer therapies (48). Loss of NIS protein 514 expression at the basolateral membrane of thyrocytes is a well-accepted precursor for reduced effectiveness of I¹³¹ therapy, as demonstrated in poorly differentiated and 515 516 undifferentiated thyroid cancers (49,50). Therefore, it was necessary to assess the 517 expression of NIS in thyroid explants which had been subjected to 96hr within the 518 microfluidic device and elucidate whether its expression was altered. Western blot 519 data revealed that there was no significant change in terms of NIS protein levels 520 caused by culture within the PCTS device, indicating that the system is valid for the future testing of I^{131} sensitivity. 521

522 T4 is exclusively synthesised by thyrocytes as a pro-hormone, which becomes 523 de-iodinated within target tissues to produce the more biologically potent T3 (51). 524 This natural phenomenon allowed the measure of T4 release from on-chip PCTS to be investigated as a measure of tissue functionality. Loss of, or reduced functional 525 526 differentiation, occurs in all thyroid carcinomas leading to diminished expression of 527 proteins central to thyroid hormone production (52). In the current study, benign tissue produced a significantly higher volume of T4 than malignant tissue throughout 528 529 the culture period, agreeing with the notion that malignant thyroid tissue has a 530 decreased ability to produce hormone (11). Detection of T4 within culture supernatant 531 strongly suggests that thyroid hormone was synthesised de novo by on-chip thyroid 532 tissue and that essential components such as I⁻ are reaching the thyrocytes. In the 533 clinical setting, the thyroid hormone precursor TG is used as a specific marker of remnant tumour tissue after thyroid removal (53). As our intention was to demonstrate 534 535 thyroid tissue functionality, we decided to measure T4 levels as T4 synthesis relies on the success of additional mechanistic steps such as cellular I uptake and TG 536 537 iodination.

538 Conclusion

Results reported in this work validate the use of a PCTS device for the 539 540 maintenance of ex vivo thyroid tissue which can be used for customising drug 541 treatment. It is proposed to use the system described to delineate sensitivity of patients suffering from thyroid carcinoma to treatment with ¹³¹I, enabling patient stratification 542 543 and reducing incidence of inappropriate treatment, reducing patient morbidity, whilst saving NHS resources. This is the first study of its kind to demonstrate reliably the 544 545 maintenance of viable ex vivo thyroid tissue for up to 96hr, with pre- and post-culture 546 tissue showing high uniformity in terms of morphology, viability and functionality.

547 Abbreviations

TC: thyroid carcinoma; PTC: papillary thyroid carcinoma; FTC: follicular thyroid
carcinoma; DTC: differentiated thyroid carcinoma; I¹³¹: radioactive iodine; NIS:
sodium-iodide symporter; TPO: thyroid peroxidase; TKI: tyrosine kinase inhibitor;
IHC: immunohistochemistry; RT-PCR: real time-polymerase chain reaction; mRNA:
messenger ribonucleic acid; BSA: bovine serum albumin; PCTS: precision cut tissue
slice; PEEK: polyether ether ketone; ETFE: ethylene tetrafluoroethylene; PBS:

554	phosphate buffered saline; BrdU: bromodeoxyuridine; OCT: optimal cutting
555	temperature; LDH: lactate dehydrogenase; DCP: dead cell protease; T4: thyroxine;
556	TMB: 3,3',5,5'-Tetramethylbenzidine; HCl: hydrochloric acid; DAB: 3, 3 –
557	diaminobenzidine; TTF1: thyroid transcription factor-1; TG: thyroglobulin; DNA:
558	deoxyribonucleic acid.

559 **Declarations**

- 560 Ethics approval and consent to participate
- 561 The project had received ethical approval from North East-Newcastle and North
- 562 Tyneside Research Ethics Committee (15/NE/0412) and was approved by Hull and
- East Yorkshire NHS Trust R&D (R1925).

564 **Consent for publication**

565 Not applicable.

566 Availability of data and material

567 All data is provided within the manuscript.

568 Competing interests

569 The authors declare that they have no competing interests.

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571 AR received a University of Hull Allam studentship.

572 Authors' contributions

573 AR, VG, and RC undertook the experimental work; AR, JE, VG and JG designed the 574 project; GM and JE collected the thyroid specimens and relevant clinical data; LK 575 provided the histological analysis. JG is responsible for guaranteeing the data. All 576 authors approved the final version of the manuscript.

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- 583

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745

746 Figure Legends

747 Figure 1: PCTS Culture device. A: Photograph illustrating device assembly. Two 748 polyether ether ketone (PEEK) plastic plates, each with a medial recess to house a sintered pyrex disk, affix to sandwich a silicone gasket with a central cavity in which 749 750 the precision cut tissue slice (PCTS) is contained. A 70µM porous nylon membrane 751 separates the tissue from the sintered disk (not shown). B: Photograph of an 752 assembled PCTS culture device with external dimensions. C: Schematic of PCTS 753 culture device. Component parts numerically labelled: 1, PEEK plastic plates; 2, glass sintered pyrex disk; 3, central silicone gasket; 4, tumour tissue sample. 754

Figure 2: Haematoxylin and eosin stained 8µM frozen thyroid sections.
Representative images from two patients A and B. Top: fresh tissue frozen prior to
culture. Bottom: tissue frozen subsequent to 96hr culture within the PCTS device.
Images are shown at both 100x and 400x magnification.

759 Figure 3: Measurement of lactate dehydrogenase (LDH) and dead-cell protease (DCP) release into culture effluent for the evaluation of cell membrane damage. 760 761 A: Lactate dehydrogenase release from both malignant and benign thyroid tissue (n=14 and n=10, respectively unless otherwise stated; relative absorbance of formazan 762 reaction product) during on-chip culture of thyroid tissue normalised per mg starting 763 764 tissue wet weight. B: Level of relative light units (RLU) produced as a result of cleavage of the luminogenic assay substrate by dead cell protease released per mg of 765 766 on-chip thyroid tissue over the 96hr culture period (n=11). Lysis buffer (10% v/v) was 767 added to homogenised tissue after 96hr culture (arrow) in order to purposefully rupture cell membranes and induce complete release of remaining LDH/ DCP. 768

Figure 4: Cellular viability and apoptosis in freshly resected, control and treated 769 thyroid tumour tissue. Cellular ability to prevent both PI (A) and TB (B) transit 770 771 across the plasma membrane was employed as a proxy of viability (n=3, mean+ SEM). No significant difference was observed between fresh and untreated control thyroid 772 tissue. C: Terminal deoxynucleotidyl transferase dUTP nick end labelling in both 773 774 fresh (+0h) and post-culture (+96hr) malignant thyroid tissue explants demonstrated no difference in the proportion of apoptotic cells in post-culture specimens (n=9; 2.78 775 776 vs. 5.59%, p=0.51 [paired t-test]). Treatment of cultured thyroid explants with etoposide and SP600125 resulted in a significant increase in apoptosis (15.25% and 777 778 14.24%, respectively) which were both significantly increased compared to untreated explants (n=5; p = <0.001). **D:** Representative images of both pre-MF and untreated 779 780 post-MF thyroid explants illustrating apoptotic cells (FITC; green) counterstained with DAPI (blue). 781

Figure 5: Percentage Ki-67 positivity in fresh (+0h) and post-culture (+96hr) 782 thyroid tumour tissue. Mean Ki-67 positivity was 1.52 ±0.52% and 1.3 ±0.34% in 783 fresh and post-culture tissue, respectively; no significant difference was observed 784 (n=8; p=0.32 [paired t-test]). Inset: Representative photomicrographs of Ki67, BrdU 785 786 and TTF1 positive brown nuclei and counterstained with haematoxylin (x400). BrdU 787 staining is only shown in cultured tissue due to the requirement of perfusion with the 788 molecule in order to elicit its incorporation and subsequent detection; 12.09 ±4.38% 789 cells stained positive for BrdU incorporation (n=3).

Figure 6: Assessment of sodium iodide symporter (NIS) protein expression by Western blotting. Band densitometry confirmed that NIS expression was not significantly altered by the microfluidic culture of thyroid tumour tissue explants (n=5). [+] and [-] represent protein extracted from tumour tissue with and without onchip culture respectively. 1-5 indicates five separate patient samples and K1 is protein extracted from the thyroid cell line. Figure 7: Thyroxine (T4) release by on-chip thyroid tissue. Concentration of T4 in effluent samples collected throughout the culture of both malignant (n=7) and benign (n=7) thyroid tissue explants on the PCTS device. Overall T4 release by benign thyroid tissue was significantly higher than that of malignant thyroid tissue (p=0.03; 2-way ANOVA). Results normalised mg⁻¹ tissue.