

1 **Procoagulant tumour microvesicles attach to**
2 **endothelial cells on biochips under microfluidic**
3 **flow.**

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22 **Abstract**

23 Tumour patients are at a high risk of venous thromboembolism (VTE) and the mechanism by
24 which this occurs may involve tumour derived microvesicles (MV). Previously, it has been
25 shown that tumour MV become attached to endothelial cells in static conditions. To investigate
26 whether this process occurs under physiologically relevant flow rates, tumour MV were perfused
27 across a microfluidic device coated with growing human umbilical endothelial cells (HUVECs).
28 Cell lines were screened for their ability to form tumour spheroids and two cell lines, ES-2 and
29 U87 were selected, formed spheroids were transferred to a microfluidic chip and a second
30 endothelial cell biochip was coated with HUVECs and the two chips linked. Media was flowed
31 through the spheroid chip to the endothelial chip and procoagulant activity (PCA) of the tumour
32 media was determined by one-stage prothrombin time assay.
33 Tumour MV were also quantified by flow cytometry before and after interaction with HUVECs.
34 Confocal images showed HUVECs acquired fluorescence from MV attachment. Labelled MV were
35 proportionally lost from MV rich media with time when flowed over HUVECs and was not
36 observed on a control chip. The loss of MV was accompanied by a proportional reduction in PCA.
37 Flow cytometry, confocal microscopy and live flow imagery captured under pulsatile flow
38 confirmed an associated between tumour MV and HUVECs. Tumour MV attached to endothelial
39 cells under physiological flow rates which may be relevant to the VTE pathways in cancer
40 patients.

41 **Keywords:** thrombosis; microparticles; microvesicles; endothelium

42

43 Introduction

44 Microfluidic technology is already showing potential in areas related to medicine and medical
45 diagnostics through the manipulation of biological samples and the use of miniaturized devices ¹.
46 Microfluidic culture systems are able to function, assess, and provide data for nanoenvironments
47 through their ability to mimic *in vivo* biological systems onto closely resembling *in vitro* microfluidic
48 environments ². Moreover, microfluidics has the ability to handle microliter volumes in
49 microchannels of 1 μm to 1000 μm and where fluid flow is strictly laminar and concentrations of
50 molecules can be well-controlled. Since the early 1990s, this technology has been used to for
51 biological research methods for specific analyses such as polymerase chain reaction and DNA
52 microarrays and also appears to be an ideal tool for the study of cancer ³. As such microfluidics
53 has been utilised to study tumour biopsies.

54 Tumours are known to release subcellular extracellular vesicles (EV) composed of both larger (100-
55 1000 nm) microvesicles (MV) and nano-sized exosomes (<100nm) into the bloodstream ^{4,5}. MV are
56 shed from cells via a number of pathways such as apoptosis and membrane remodelling ^{6,7}. MV are
57 released into the circulation where they can then be detected in blood samples using a standardised
58 flow cytometry technique ⁸. MV were originally thought to be simply inert cellular debris but they
59 have been found to play a number of roles depending on their parent cells and the antigens they
60 retain from the parent cells ^{9,10}. Target cells are modulated by MV through their capacity to facilitate
61 cell-to-cell interactions, where proteins and mRNA are transferred to neighbouring cells, raising the
62 expression of protein on the target cell membrane and inducing cell signalling ^{11,12}. MV have been
63 implicated in the prothrombotic state associated with cancer and Tissue Factor (TF)-bearing MV
64 (TFMV) in particular are found in cancer patients' plasma and have been suggested as a possible
65 risk factor for occurrence of venous thromboembolism (VTE) ¹³.

66 Many tumour cells express TF, especially cancers that originate in the epithelium and TFMV are
67 spontaneously released into the circulation by these tumours ^{14,15}. TF is a trans-membrane, 47-KDa-
68 glycoprotein¹⁶ and the key activator for haemostasis, serving as the protein component of tissue
69 thromboplastin ¹⁷. TF also play a vital role in a number of cellular processes including intracellular
70 signalling, cell proliferation, and blood vessel development ¹⁸.

71 TFMV are found in the blood of healthy individuals ¹⁹ as well as those with cancer, but levels tend
72 to be higher in cancer patients and this has been recorded in a number of malignancies including
73 breast cancer ²⁰, colorectal cancer ²¹, and pancreatic cancer ^{22,23}. Together, these results suggest the
74 potential of TFMV as a biomarker identifying among cancer patients those who are a high
75 thrombosis risk ^{24,25}. The procoagulant potential of TFMV mostly dependent on the presence of TF
76 which can drive coagulation²⁶ and also anionic phospholipid expression, particularly
77 phosphatidylserine (PS). Lacroix and Dignat-George (2012) describe MV that contain both PS and
78 TF as particularly procoagulant ²⁷ and a significant number of prothrombotic conditions have been
79 reported to have elevated MV numbers in plasma ²⁸.

80 A number of studies have also found links between TFMV and thrombosis using *in vivo* mice
81 models. One such experiment by Thomas et al. ²⁹ involved infusion of MV derived from cancer cells
82 that showed an accumulation at the injury site as well a reduction in tail bleeding time and the time

83 of arterioles and venules occlusion. The study showed that MV derived from cancer cells and
84 carrying TF and P-selectin glycoprotein ligand 1 (PSGL-1) were active in forming an *in vivo*
85 thrombus²⁹. The shedding by a tumour of TF-bearing MV through leaking blood vessels in the
86 tumour mass, tumour-induced upregulation of TF expression in monocytes and endothelial cells,
87 and upregulation of endothelial cell TF expression by chemotherapeutic agents together lead to
88 elevated circulating TF levels³⁰. Tumours which are sensitive to chemotherapy would be more
89 likely to cause VTE, given that such tumours are more likely to shed greater numbers of MV via
90 apoptosis³¹. Involvement of TF in tumour progression has also been demonstrated via
91 hematogenous metastasis^{32,33}. *In vitro* data has also confirmed a role for TFMV in coagulation and
92 thrombin-generation^{34,35} and they have been shown to promote metastasis through angiogenesis,
93 immune suppression, cancer cell survival, and invasion¹³. All of these processes require the ability
94 to interact with the endothelium.

95 A microfluidic device has been shown previously to be capable of extracting antigen-specific MV
96 from biologically complex samples, such as serum and conditioned medium from cultured cells.
97 The majority of MV isolated via this method retained their native morphology³⁶. Wu et al.
98 developed a microfluidic platform that first filters red blood cells out from blood and then further
99 analyses the remaining vesicles based on their smaller size; this way, over 99% of RBCs can be
100 removed from the initial sample, and the exosomes with desired size were further purified with an
101 efficiency of over 98%³⁷. Therefore, microfluidic devices are ideal candidates to study translation of
102 biomarkers such as tumour MV to study clinically relevant questions.

103 The purpose of this present work is to investigate how tumour MV are able to interact with
104 endothelial cells *in vitro* utilising a microfluidic platform. Understanding more fully the
105 mechanisms of endothelial involvement in thrombotic events may help in the development of
106 better therapeutic solutions in cancer management.
107

108 **Materials and Methods**

109 *Cell lines and culture*

110 The ovarian carcinoma cell line ES2 (ATCC, UK) and glioblastoma U87 cell line (ATCC, UK were
111 seeded at 1×10^6 /ml cells into 25 cm² tissue culture flask (Sarstedt, UK) and left to adhere overnight
112 at 37°C in a 5% CO₂ incubator and maintained in McCoy's 5A media or DMEM media respectively,
113 supplemented with 10% (v/v) Foetal Bovine Serum (FBS) and 1% (v/v) Penicillin/Streptomycin (all
114 Lonza, UK). Spheroids were formed using ultra low adherence 96-well plates (ThermoFisher, UK)
115 seeded with 2×10^5 cells and cultivated over 5-7 days prior to use. Primary Human umbilical vein
116 endothelial cells (HUVECs; PromoCell, Heidelberg, Germany) were cultured in complete
117 endothelial cell growth media (ECGM, PromoCell). HUVECs were seeded at 1×10^6 /ml cells into 25
118 cm² cell+ tissue culture flasks (Sarstedt) and cultured at 37°C in a 5% CO₂ incubator. HUVECs were
119 utilised at passages 3-6.

120 *Procoagulant activity*

121 The procoagulant potential of cell-free supernatant and cells were measured using the semi-
122 automated Thrombotrack SOLO coagulometer. This machine works by mechanical detection of the
123 clotting endpoint method. Samples (100µl) were placed into a cuvette containing a steel ball and
124 25mM CaCl₂ (100µl) was added; finally, 100µl of control plasma (NormTrol, Helena Biosciences,
125 UK) was added and the time taken for clot formation (prothrombin time, PT) was automatically
126 determined.

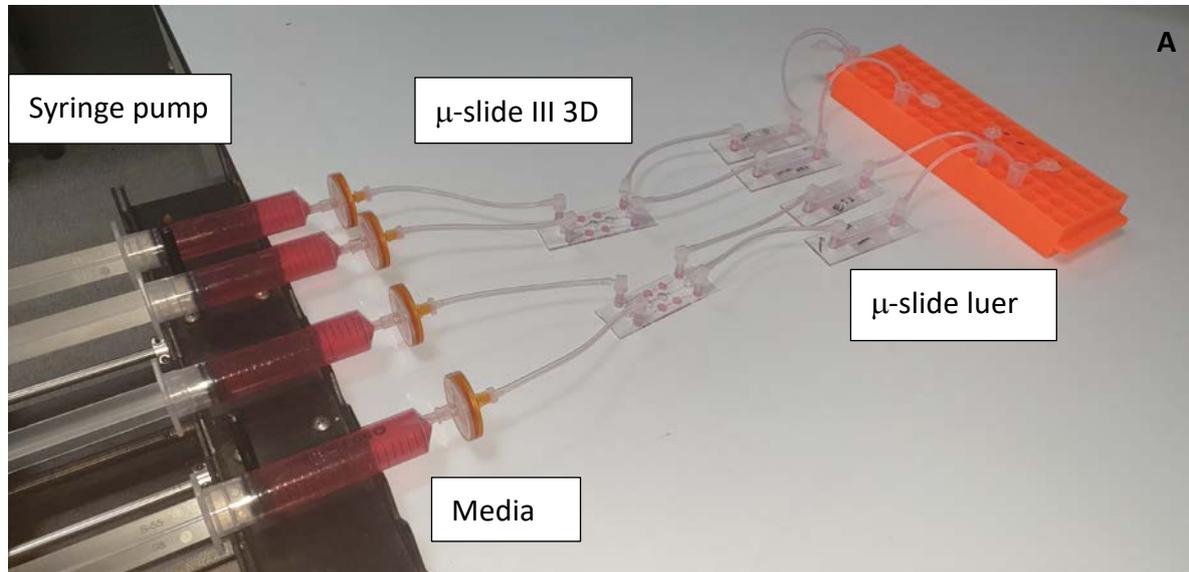
127 *CFSE staining protocol*

128 MV released from ES-2 and U87 tumour cells were labelled via 5(6)-carboxyfluorescein diacetate N-
129 hydroxysuccinimidyl ester (CFSE) staining of the parent cells. Harvested cells (1×10^6 cells/ml) from
130 ES-2 and U87 cancer cells were suspended in 1 ml PBS and incubated with CellTrace™CFSE dye
131 (Invitrogen, UK) at 5µM as a final working concentration and incubated for 20 minutes at room
132 temperature or 37 °C in the dark. Stained cells were washed twice with PBS and seeded into a series
133 of 25 cm² cell culture flasks in 10 ml of the appropriate medium and incubated for 24 h at 37°C and
134 5% CO₂. Unlabelled cells were used as negative control.

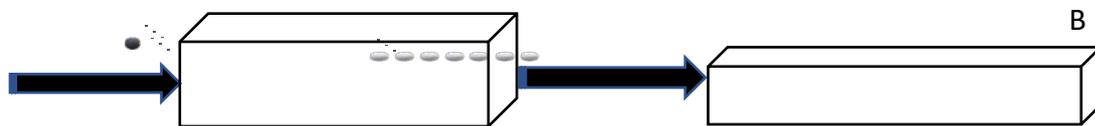
135 *Microfluidic chips*

136 Two chips were used for HUVECs experiments, either a µ-Slide I Luer (Ibidi, Germany) or a Vena8
137 endothelial cell biochip (Cellix, Ireland). Slides were treated with UV irradiation for 20 minutes and
138 coated by dispensing approximately 12 µL of type B 2% v/v gelatin (Sigma Aldrich, UK) into the
139 channel. Control chips were also treated in the same way to account for non-specific binding. Then,
140 the biochips were then incubated for 24 hours at 4°C. Cultured HUVECs (2000 cells) were added
141 into each channel and the reservoirs filled with 60µL of media. The biochips were incubated in the
142 CO₂ incubator for 24 hrs at 37°C. Then, labelled/unlabelled MVs were perfused over the HUVECs
143 for 6 hours and PCA, MV quantification and microscopy images were assessed to evaluate MV
144 interaction with HUVECs. Control chips without HUVECs were done in parallel to the
145 experimental setup.

146 A μ -slide III 3D perfusion was used to hold the spheroids then flow was applied via a syringe
147 pump (4 μ L/min). A μ -Slide I Luer, which was precoated with HUVECs and was attached to the
148 output of the μ -slide III 3D chip as shown in Figure 1a and b. Samples were then collected via the
149 output of the μ -Slide I Luer into sterile 1.5ml polypropylene tubes.



150
151 **Figure 1a.** Basic experimental setup showing tumour fresh media contained in syringes linked to a multiwell
152 μ -slide III 3D chip containing either ES-2 or U87 spheroids linked through to a μ -Slide I Luer containing
153 HUVECs and finally sample collection tubes. The experiments were carried out in a 37 °C incubator.



154
155
156 **Figure 1b.** Schematic of experimental setup. Media was flowed via either syringe pump (constant flow) or
157 Kima pump (pulsatile flow) through a microfluidic chip containing tumour spheroids. MV are released from
158 the spheroids into the media which is then connected to a second chip coated with HUVECs to study their
159 interaction.

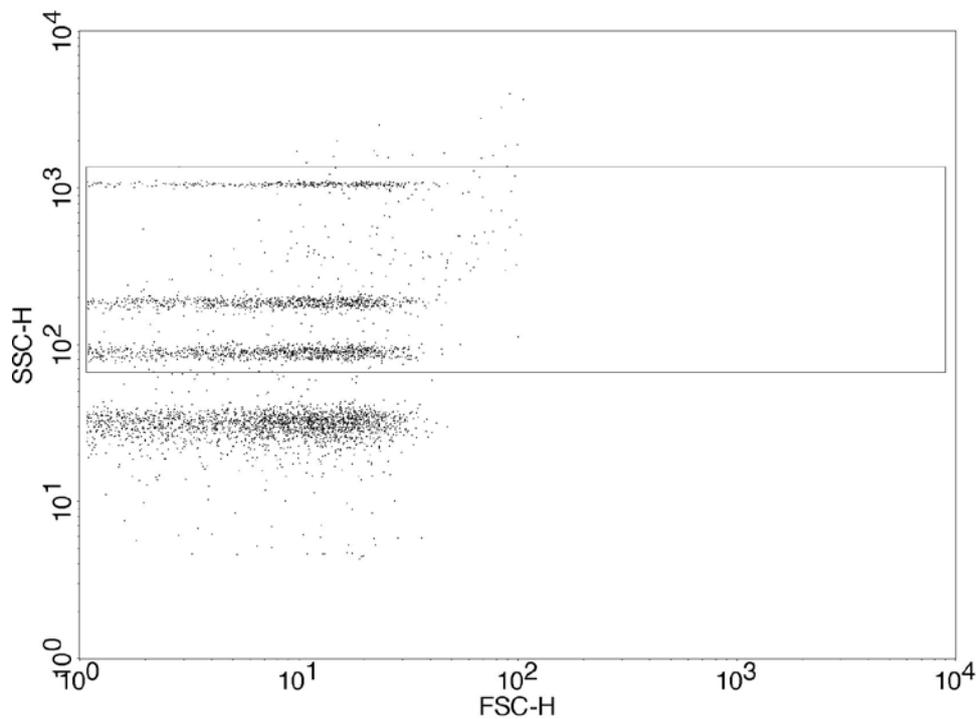
160 Ultrafiltration

161 CFSE labelled-MV cell free media was harvested from ES2 and U87 cells and centrifuged at 300 g at
162 4°C for 4 minutes to remove detached cells. Supernatant (6ml) was collected and filtered through
163 Vivaspin® 6 ml concentrators (Sartorius, UK). MV were recovered from the media concentrate and
164 PCA was assessed. The molecular weight cut off was 100kDa; MVs were presumed not to pass
165 through as filtrate due to their relatively large size in comparison to the cut off value.

166 Flow cytometry

167 CFSE Labelled MVs released from ES2 and U87 tumour cells were quantified by flow cytometry
168 before and after being passed through the biochip. Samples (50 μ l) of labelled (either CFSE or anti-
169 TF: FITC (Bio-rad)) and unlabelled samples were immediately analysed by flow cytometry by
170 adding an equal volume of Accucheck beads (Invitrogen, UK) and 150 μ l of 0.2 μ m-filtered sterile

171 PBS. Unlabelled MV samples were used as negative control. A flow cytometer (BD FACSCalibur)
172 was setup with Megamix SSC beads (Biocytex, France) that are used to define a MV gate according
173 to side-scatter characteristics of the beads (Fig. 2) following the manufacturer's protocol.



174
175 **Figure 2.** Defined MV gate based on Megamix SSc beads manufacturer protocol. The box around the 3
176 differentially sized Megamix SSc beads on side scatter represents the MV gate set at approximately 0.2 to 0.5
177 μm . The lowest SSc beads are $0.16\mu\text{m}$ and do not form part of the MV gate.

178 Microscopy

179 The μ -Slide I Luer microfluidics biochip were coated with HUVECs cells and washed twice with
180 PBS to investigate the immobilization of (CFSE)-labelled MVs. Labelled/unlabelled MVs of ES2 and
181 U87 cell free medium were perfused over the HUVECs for 6 hours. Confocal microscopy was
182 performed using a Zeiss LSM710 Laser Scanning Confocal Microscope and images acquired using
183 ZEN software (Zeiss Group, Oberkochen, Germany).

184
185 The interaction of MV on HUVECs was further studied using an automated microfluidic platform
186 (VenaFlux and Vena8 Endothelial+ biochips; Cellix, Dublin, Ireland) in order to mimic
187 physiological flow status. The Vena8 chip was coated with HUVECs (same conditions as previously
188 described) and connected to a Kima pump (Cellix) which delivers pulsatile flow with shear stress at
189 $450\mu\text{l}/\text{min}$ for 6 min, followed by 5 min of absence of flow. The flow chamber was then connected to
190 the Mirus Evo Nanopump (Cellix) and the channels were rinsed three times with $25\mu\text{l}$ of media
191 prior to each experiment, and MV adhesion was initiated by the addition of CFSE-labelled MV
192 supernatant of (ES-2 and U87) and unlabelled MV as well. Interaction of MV was recorded every
193 second under a shear stress of $1\text{ dyne}/\text{cm}^2$ in phase contrast and the settings were equal in all
194 conditions (exposure time 344 ms , magnification $32\times$) for 5 min.

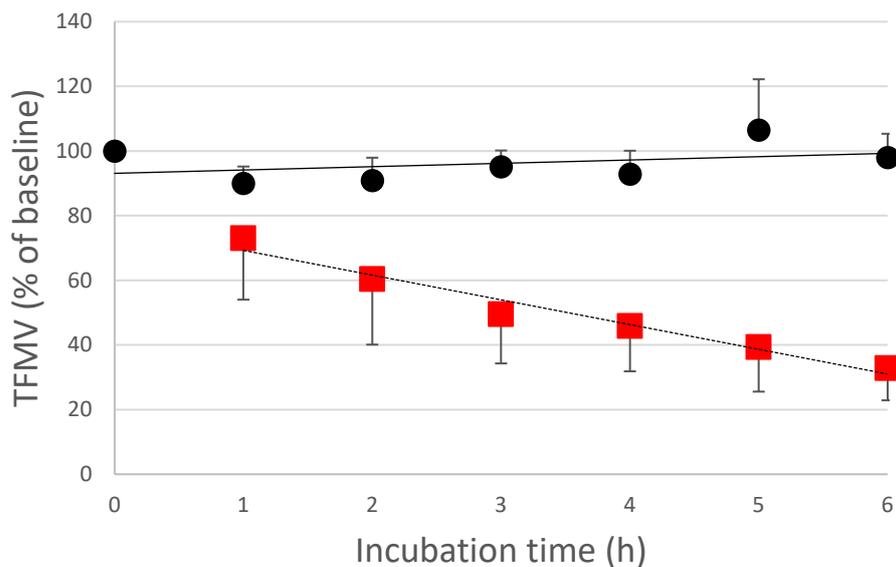
195 **Results**

196 *Procoagulant activity*

197 PCA of ES-2 and U87 cells and media were assessed via the one stage PT assay. For the same
198 concentration of cells within the assay (3×10^5) the PT was similar between the ES2 (33.0s) and U87
199 (32.6s). The cell free media harvested at the same time was shown in both cells line to be
200 procoagulant with ES-2 media supporting a PT of $76.9 \pm 3.4s$ (n=4) and U87 media was less
201 procoagulant with a PT of $137.1 \pm 4.3s$ (n=4). Ultracentrifugation using a Vivaspin (100 kDa MWCO)
202 was shown to remove all associated PCA of the filtrated media confirming that the PCA was MV
203 associated whereas the concentrate diluted with fresh media to the original volume was shown to
204 retain and slightly increase PCA (ES2; $41.4 \pm 9.2s$, U87; $112.8 \pm 13.3s$).

205 *TF labelling of MV and interaction with HUVECs*

206 Initially, TF labelling (anti-human TF: FITC) of MV from media of ES-2 and U87 spheroids cultured
207 on a μ -slide 3D chip was used to quantify the interaction with HUVECs under flow and the
208 relationship between TFMV with PCA. Over a time course of 6h TFMV linearly decreased (through
209 1-6h) from the media collected after perfusion across HUVECs on a μ -slide luer chip when
210 compared to a coated control chip containing no HUVECs (Fig. 3).

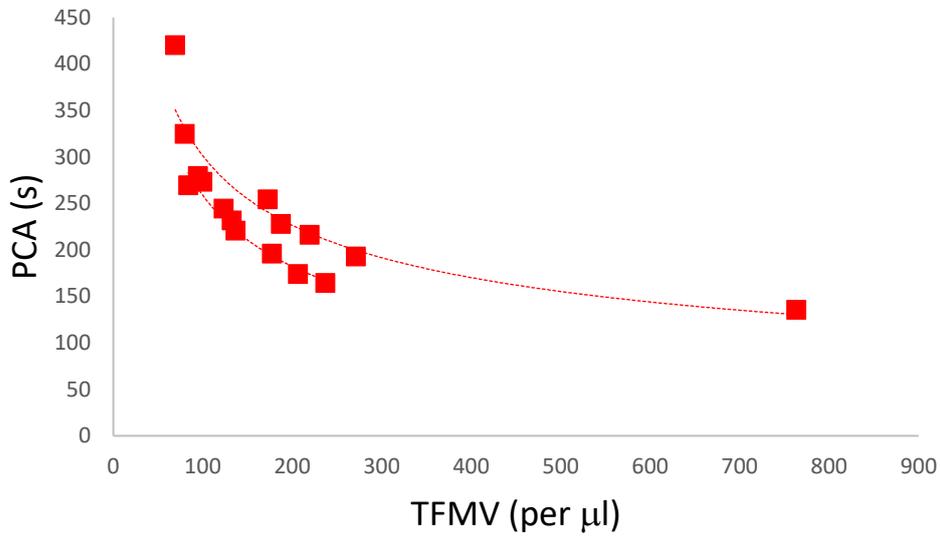


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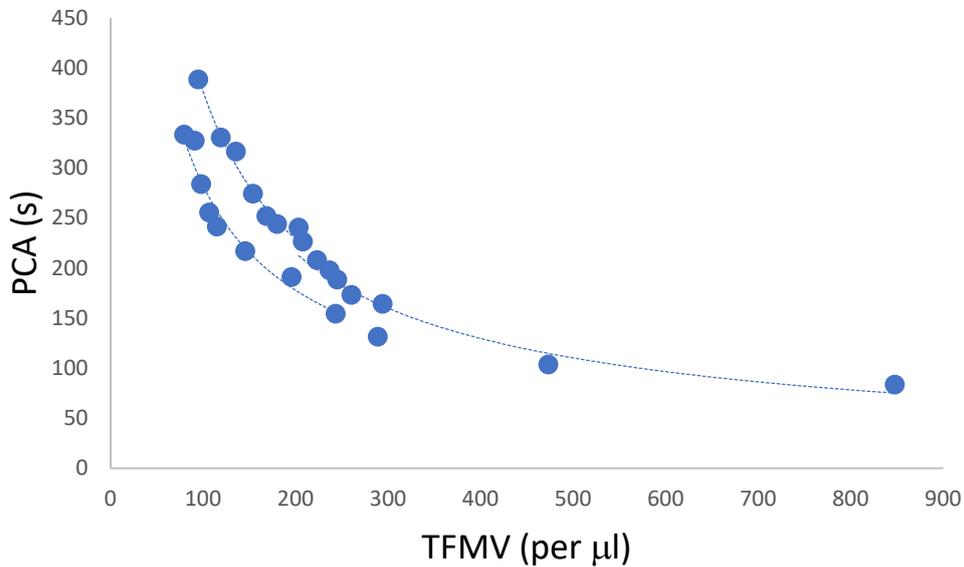
212 **Figure 3.** TFMV of ES-2 and U87 as a percentage of baseline values (n=8) when perfused across a μ -Slide I
213 Luer containing cultured HUVECs (red square) or a gelatin control chip (black circle) with no HUVECs
214 present (n=4) for 6h. Error bars are SD.

215
216 The loss of TFMV after perfusion across HUVEC coated slides was further investigated through
217 analysis of the PCA associated with the media following perfusion across the 6h time frame. A
218 clear power relationship was observed between TFMV and PCA for both cell lines and the
219 subsequent loss of detected TFMV over time with HUVECs perfusion resulted in a slower PCA (Fig
220 4). Control samples of MV rich tumour media passed through gelatin coated μ -slide luer chips

221 showed no change in PCA across the 6h experimental window (ES-2; 224.7±4.8s, U87; 190.2±7.4s)
 222 HUVECs were analysed by flow cytometry for TF expression post-perfusion and showed a mean
 223 fluorescent ratio (fluorescent intensity_{TF}/fluorescent intensity_{negative control}) increase relative to
 224 control HUVECs (ratio of 1) to 2.41±0.13 for HUVECs perfused with ES-2 MV and 2.16±0.26 for
 225 HUVECs perused with U87 MV (n=4).
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 227



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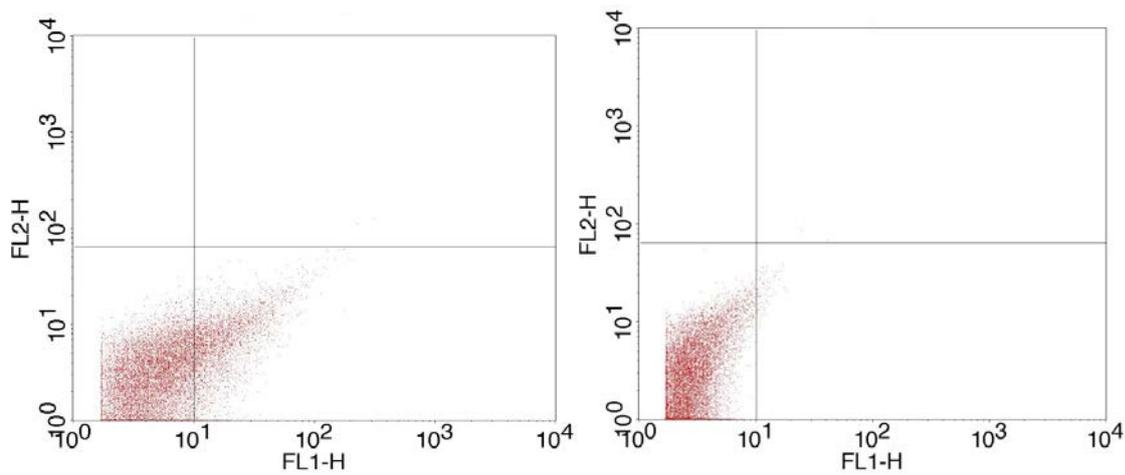
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230 **Figure 4.** Relationship between TFMV and PCA of U87 (red square, n=16) and ES-2 (blue circle, n=24)
 231 media when perfused over HUVECs for 6h. Lines of best fit are for a power relationship and R² values range
 232 from 0.904-0.985.

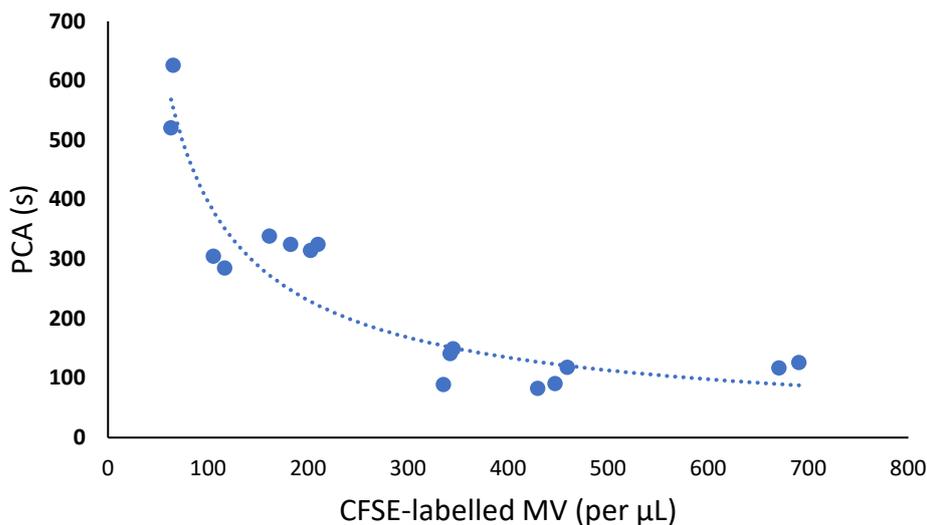
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235 *CFSE Labelling and detection of tumour MV*
 236 To visualise the observed interaction between MV and HUVECs under flowing conditions, ES2 and
 237 U87 (1×10^6 cells/ml) were fluorescently labelled with CFSE and incubated for 24 h. Cell free media
 238 from each tumour cell line was then harvested and perfused over HUVECs adhered to a
 239 microfluidic chip (μ -Slide I Luer) for 6h (equating to approximately 6.7×10^5 total MV). PCA and MV
 240 quantification was determined before and after being perfused over HUVECs. The MV gate was
 241 defined using Megamix SSc beads and CFSE-labelled MV could be clearly identified on a
 242 fluorescence plot in comparison to unlabelled MV (Fig. 5). Independent measurements showed a
 243 relationship between PCA and the quantity of CFSE labelled MV (Fig. 6).

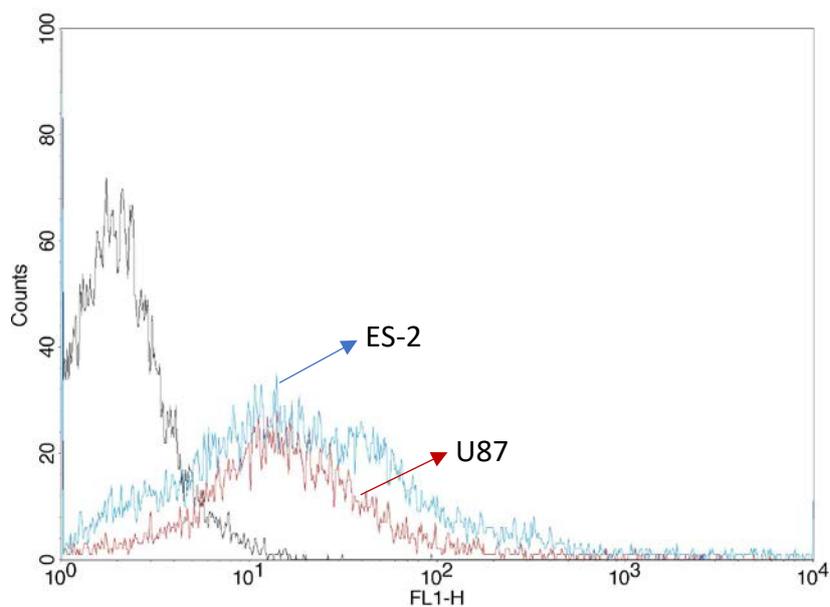


244
 245 **Figure 5.** CFSE fluorescently labelled (left panel) and unlabelled (right) MV populations. The individual MV
 246 events in the lower right quadrant correspond to CFSE-labelled MV (increased FL-1 signal) which were then
 247 quantified using counting beads.



248
 249 **Figure 6.** The correlation between CFSE- labelled MV with PCA of tumour media ($n=16$, independent
 250 measurements)
 251

252 HUVECs were detached from the μ -Slide I Luer chip at the end of the 6h period and analysed for
253 PCA and the acquisition of fluorescent properties from the CFSE labelled MV. The PCA of HUVECs
254 (3×10^5 per assay) incubated with ES2 tumour media was 149 ± 0.5 s and 127 ± 1.2 s for HUVECs
255 incubated with U87 tumour media. The PCA of HUVECs with fresh (no TFMV) media was
256 370 ± 17.5 s. The cells were further characterised by flow cytometry and the results showed an
257 increased fluorescence (gained from labelled tumour MV) for HUVECs compared to the control
258 cells (Fig. 7). The mean fluorescent ratio of HUVECs relative to control increased to 10.52 ± 1.77 for
259 HUVECs perfused with ES-2 CFSE labelled MV and 7.53 ± 0.64 for HUVECs perfused with U87 MV
260 (n=3).



261
262 **Figure 7.** Representative (n=3) histogram plot of fluorescence of HUVECs perfused with U87 or ES-2 MV
263 rich media for 6h, compared to HUVECs perfused with control media (left peak). MV were labelled with
264 CFSE from the parent cell.
265

266 *Confocal microscopy*

267 To further define the MV interaction with HUVECs, CFSE-MV labelled were perfused over
268 HUVECs on a μ -Slide I Luer channel for 6h then washed and analysed by confocal microscopy (Fig.
269 8). Images obtained showed fluorescence localised at the surface of HUVECs.

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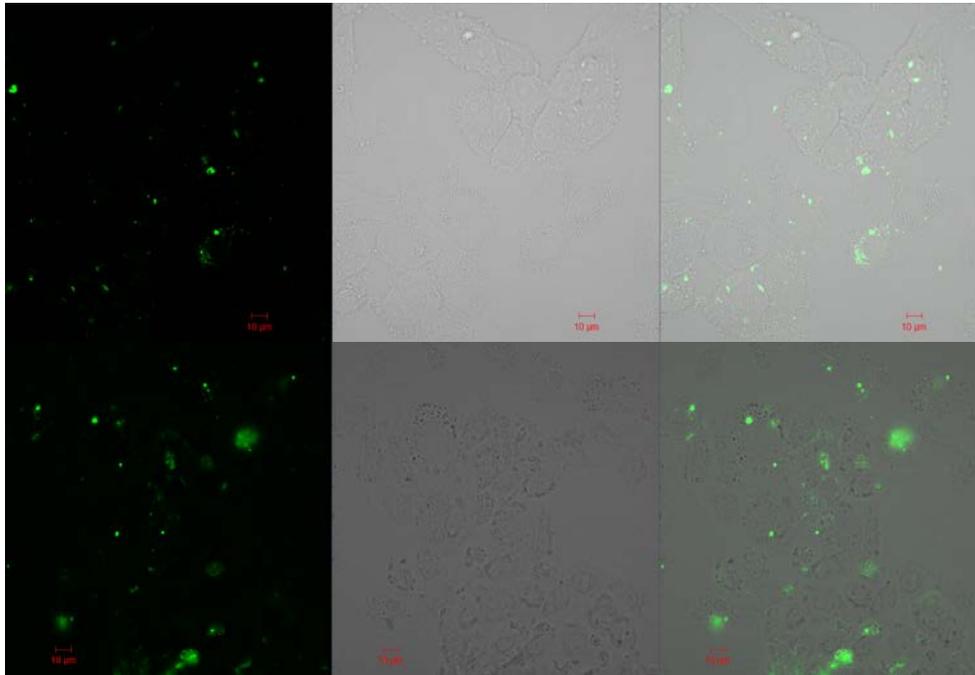
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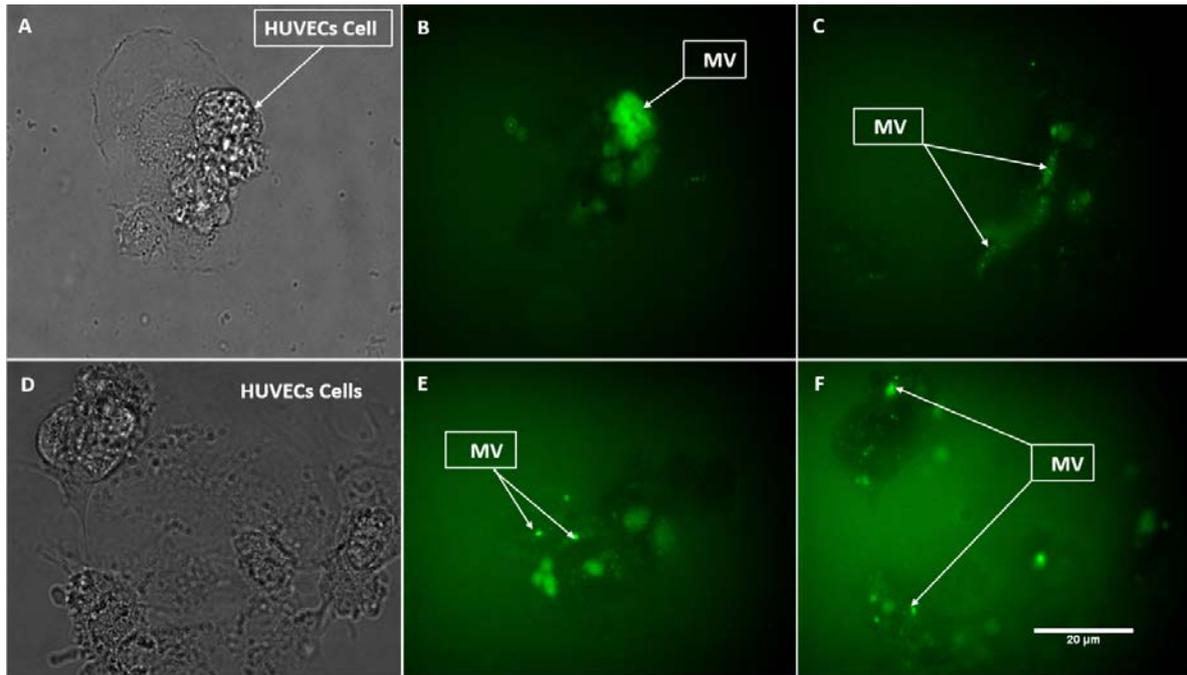


281 **Figure 8.** *Confocal microscopy of HUVECs incubated on a μ -Slide I Luer perfused with tumour media (ES-2*
282 *top panels, U87 bottom panels) with CFSE labelled MV. The left panels correspond to the fluorescent*
283 *detection channel, middle panels are brightfield detection channel and the right panels are the combined*
284 *images.*

285 *Automated image capture under flow*

286 The Cellix system allows for live image capture under physiological flow conditions and was
287 utilised to further confirm that the association of tumour MV with HUVECs, observed by confocal
288 microscopy was not due to any period of static flow between the experiment and analysis. CFSE-
289 MV were constantly passed over a Vena8 microfluidic chip precoated with HUVECs and images
290 captured 'as live' under flowing conditions. MV were again observed to associate with HUVECs
291 (Fig. 9).

292



293
 294 **Figure 9.** Still images captured from a live recording showing CFSE labelled MV aggregated on HUVECs
 295 under flow. The top panel (A-C), shows labelled ES-2 MV deposition. Image A shows HUVECs cell with
 296 unlabelled ES2-MV. Images B and C show two different MV deposition with HUVECs. Image D shows U87
 297 unlabelled-MV with HUVECs. Images E and F represents the labelled U87 MV deposition on HUVECs.

298

299 **Discussion**

300 In this study, we demonstrate for the first time that MV formed *in vitro* from tumour spheroids
 301 interact with endothelial cells under flow conditions in a dual microfluidic chip assembly. After
 302 initially adhering to the HUVEC surfaces in a static condition, TFMV were shown to associate with
 303 HUVECs under dynamic flow conditions in a time dependent manner. The correlation of loss of
 304 PCA and reduction in detected TFMV when tumour media was passed over HUVECs under flow
 305 suggests direct evidence for PCA being determined by TFMV concentration and also that TFMV are
 306 lost due to their association with the endothelial cells. Control chips coated with gelatin but
 307 without HUVECs showed no loss of MV or PCA through the experiments therefore the observed
 308 loss can be attributed to the interaction with HUVECs. We have previously shown that PCA is
 309 linked to tumour spent media concentration²³ in a power relationship, as also observed here for
 310 MV concentration (Fig. 4). The observation that the concentration of spent tumour media
 311 concentration and quantified MV both determine PCA suggests that the MV in tumour media are
 312 responsible for the associated PCA. Fluorescent and confocal microscopy (Figs 8 & 9) clearly
 313 showed a fluorescence attributed to the presence of CFSE-labelled MV on HUVECs within the
 314 microfluidic chip after tumour MV were perfused over the cells. From both TF and CFSE analysis of
 315 HUVECs post perfusion the ES-2 MV conferred an increased PCA and showed a greater
 316 fluorescence when compared to U87 MV suggesting more MV were associated with HUVECs. ES-2
 317 MV rich media was also found to possess a greater PCA prior to incubation with HUVECs which
 318 may be indicative of a greater MV concentration. After removal of MV from the media via

319 ultrafiltration (Vivaspin, 100kDa) the filtrate no longer supported coagulation. The pore size of
320 these filtration units would allow soluble TF to pass through (47kDa), if present in a monomeric or
321 dimeric form, and so the data suggest that the PCA associated with tumour conditioned media is
322 MV dependent as discussed above.

323 A possible limitation of the study would be whether the interaction with endothelial cells seen here
324 is ubiquitous and occurs for MV derived from any cell exposed to the circulation. However, the
325 acquisition of a more procoagulant HUVEC phenotype via the acquisition of TF expressing tumour
326 MV as shown here would be more specific to tumour derived MV. Furthermore it has been shown
327 that although flow cytometry is the currently the only standardised method ⁸ across laboratories for
328 enumeration of MV the method has a size limitation where smaller MV cannot be detected ³⁸. The
329 described methodology here, using Megamix beads creates an MV size window of detection of 0.2
330 to 0.5µm (Fig. 2).

331 The binding of procoagulant tumour MV to endothelial cells could have relevance to the *in vivo*
332 mechanism of VTE formation in cancer patients where TFMV have been proposed to be associated
333 with a high thrombosis risk ^{24, 25}. If tumour MV are able to bind to endothelial cells within the
334 circulation then this could be a basis for increased procoagulant potential. Future work should
335 focus on the exact mechanism of tumour MV binding to endothelial cells and the response of
336 endothelial cells to the stimuli in terms of activation, apoptosis or altered cell surface marker
337 expression.

338 It has been proposed that MV endocytosis by endothelial cells occurs through interaction between
339 anionic phospholipids at the MV surface and endothelial cell surface expressed $\alpha v\beta 3$ integrin ³⁹.
340 This process was shown to be inhibited in the presence of annexin V and the internalisation of MV
341 and subsequent protein digestion at the MV surface by trypsin additionally provides evidence of a
342 phospholipid role in binding of MV to endothelial cells ³⁹. The engulfment and recycling of MV
343 through the Rab family of Golgi-endosomal transport network has also been demonstrated ⁴⁰.
344 Furthermore, there is evidence of TF-VIIa-protease-activated receptor (PAR) 2 signalling in
345 thrombin generation (and activation of other trans-membrane G protein-coupled receptors) leading
346 to transcription of prothrombotic genes, signal transduction amplification cascades and also the
347 establishment of tumours ^{41, 42}. PAR1 can also trans-activate PAR2, which can promote an extra
348 thrombin generation response in the endothelium and tumour environment ⁴³.

349 When cells are exposed to inflammatory cytokines, leukocytes are more likely to undergo
350 microvesiculation, and are therefore capable of the production of TFMV, which may become
351 associated with developing thrombus via P-selectin glycoprotein ligand 1-P-selectin interactions
352 and also may stabilise the thrombus by fibrin formation induction ^{44, 45}. Neutrophils can also recruit
353 TFMV ⁴⁶, and the extracellular traps that they project have been demonstrated *in vitro* to serve as an
354 adherence site for tumour-derived TFMV ⁴⁷. This may be a significant process for localising TFMV
355 and concentrating additional TF into the developing thrombus. There is also evidence to suggest
356 that MV are able to transfer their procoagulant potential to other cell types, and in doing so can
357 exacerbate endothelial activation ⁴⁸ as suggested here. While TF expression can be induced in
358 cultured endothelial cells in response to inflammatory, *in vivo* it is probable that the TF associated

359 with endothelial cells is derived from TFMV released by monocytes or tumour cells^{49, 50}. Moreover,
360 the expression of TF on the endothelium in response to both monocyte-derived MVs and
361 inflammatory mediators accompanies the concomitant translocation of phospholipids such as PS,
362 that could enhance the binding of coagulation factors⁵¹. The induction of endothelial cell apoptosis
363 is related to MV generation and downregulation of TF pathway inhibitor, thrombomodulin and
364 glycosaminoglycans such as heparan sulphate on the endothelial surface⁵². The resultant
365 impairment of activation of the protein C anticoagulant pathway and reduced antithrombin III
366 activity may be attributed to the disrupted integrity of the endothelium. In addition, activated
367 endothelial cells express cell surface adhesion molecules which increase platelet adhesion and
368 attract monocytes and neutrophils, all of which might further contribute to coagulation initiation or
369 amplification^{53, 54}.

370 In summary we report a microfluidic two-chip setup which showed that tumour MV released from
371 spheroids bind to endothelial cell under dynamic, physiologically relevant flow conditions.

372 **Conclusion**

373 Tumour derived procoagulant MV were shown to become associated with endothelial cells under
374 flow conditions within a dual microfluidic setup. Tumour MV were shown be the cause of
375 procoagulant activity *in vitro*.

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