

- 1 1. The within-match patterns of locomotor efficiency during Professional Soccer match play:
2 Implications for Injury risk?
- 3 2. Original Investigation
- 4
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- 24 5. Locomotor efficiency during soccer match play
- 25 6. Abstract Word Count: 253
- 26 7. Word Count: 2998
- 27 8. Number of Tables and Figures: 3

53 **Introduction**

54 Monitoring load in team-sports players during training and match play is common practice within
55 industry settings in order to reduce injury risk and optimise their readiness to perform^{1,2}. Obtaining
56 measures of internal load (e.g. heart rate) during competition can be impractical and often prohibited;
57 hence practitioners tend to rely on external load measures, such as locomotor activities, to monitor
58 training and competition loads. Analyzing locomotor activities during match play has demonstrated
59 within-match patterns, with total distances covered (TDC) and high-speed running distances (HSR)
60 decreasing towards the latter stages of each half³. These time periods towards the end of each half have
61 been associated with a high injury incidence rate in professional^{4,5} and elite youth⁶ soccer players,
62 perhaps owing to fatigue⁷. Indeed, studies that have simulated soccer matches in laboratory-controlled
63 conditions have observed within-match patterns in lower limb kinematics⁸, strength,^{8,9} and motor unit
64 recruitment¹¹ that are synonymous with injury incidence trends. However, monitoring these specific
65 injury risk markers during training and competition is not feasible, and real-time surrogate measures
66 are required to enable practitioners to make informed load-monitoring judgements during matches and
67 training sessions.

68

69 Locomotor activities such as TDC and HSR can be monitored real-time with advances in time-motion
70 analysis technology; however these metrics neglect the energetically taxing changes in speed^{12,13}. The
71 change in speed has been determined as the frequency and/or distance covered in different
72 acceleration/deceleration categories^{13,14} or using more complex energetic models to estimate metabolic
73 cost^{12,16}. Whilst these contemporary methods maybe valuable additions to monitoring external load for
74 practitioners, they quantify players' positional change in a single plane of motion, neglecting soccer's
75 three-dimensional nature of movement and impacts.

76

77 Tri-axial accelerometers measure three-dimensional movements and have been used to quantify
78 external load in team sports, often determined by a vector magnitude termed PlayerLoad™ (PL_{VM}¹⁷,
79 ¹⁸). In contrast to existing metrics using time-motion analysis, PL_{VM} has an acceptable signal: noise
80 ratio¹⁹ owing to its demonstrated test-retest²⁰, within- and between-device reliability¹⁹. The within-
81 match patterns of PL_{VM} were recently examined using standardised soccer simulation under
82 laboratory-controlled conditions in which the volume and intensity of intermittent and multi-
83 directional locomotor activities were fixed in 15-min match segments²¹. In this study PL_{VM} increased
84 in the last 15-min period of each half, mirroring the within match patterns of fatigue^{9,11} and injury
85 risk^{4,5}, indicative of a change in movement strategy¹⁷ and/or a reduced locomotor efficiency²¹. Soccer
86 specific fatigue may manifest in the reduced stiffness of the musculotendon unit¹⁵, owing to a reduced
87 central motor output^{11,15}, which may compromise the absorption capacity and stability of lower-limb
88 joints²⁸, increasing the injury risk to passive joint structures. Decreased stability and increased lower-
89 limb vibrations associated with the ground reaction force in a fatigued state³⁰ may be detected with
90 high-resolution tri-axial accelerometer technology and may explain the reduced locomotor efficiency
91 observed in the latter stages of each half of simulated soccer match-play²¹.

92 However, during competitive games, within-match changes in locomotor efficiency may not be
93 detectable using PL_{VM} alone, given its strong positive association with total distance covered¹⁸. Hence,
94 PL_{VM} is hypothesised to decrease over the course of each half of match-play synonymous with the
95 decline in locomotor activity³. In this study, we primarily aimed to determine the within match-
96 patterns of PlayerLoad™ and locomotor variables in competitive fixtures; however we also attempted
97 to determine match-related changes in players' locomotor efficiency patterns by calculating a ratio of
98 PL_{VM}:TDC (or PlayerLoad™ per meter). Whilst exploratory, we hypothesised that within-match
99 declines in locomotor activities (TDC) would be greater than PlayerLoad™ metrics, an uncoupling
100 which may be identified with the application of PL_{VM}:TDC, and indicative of a reduced locomotor
101 (movement) efficiency. Furthermore, because PL_{VM} is influenced by individual gait patterns²⁰ and

102 locomotor activities¹⁸, and that match running variables are dictated by positional role²², our second
103 aim was to quantify the determinants of PL_{VM} together with its between match variability.

104

105 **Method**

106 The study gained ethical approval from a departmental ethics committee prior to the commencement
107 of the study. As these data reported as part of this retrospective study was collected as part of the
108 routine data monitoring of players in industry practice, informed consent was not deemed necessary²⁷.

109

110 Data was collected during the 2012/2013 and 2013/2014 seasons from three English Championship
111 U21 teams (Age: 20.3 ± 1.6 years; Stature: 1.80 ± 0.07 m; Body Mass: 81.2 ± 6.1 kg). Official's
112 permission was gained to wear the MEMS devices (Micromechanical Electrical Systems) prior to each
113 match, which were played on natural turf. On match day, players wore a customised tight-fitting
114 neoprene garment underneath their match day shirts, with the unit located between the scapulae. Prior
115 to MEMS device (MinimaxX S4, Catapult Sports, Melbourne, Australia) placement in the players
116 garment, units were taken outside and activated 15 mins beforehand to attenuate erroneous data owing
117 to poor GPS signal quality. All warm-up data was excluded from the study. Match play consisted of
118 two 45 min halves with a 15 min passive half-time interval. Any additional time at the end of each half
119 was excluded from the analysis given the between-match variation in duration. Only players
120 completing three full 90 min games were included in the study, to permit the assessment of between
121 match-variation in our outcome measures. Sixty-four professional soccer players were included in the
122 study, which provided 574 match observations from 86 games (Team 1, n= 221; Team 2, n=196;
123 Team 3, n= 156). These match recordings were then dissected into 15 min periods to assess the within-
124 match patterns of PL_{VM} and the individual accelerometer planes. In accordance with previous time-
125 motion analysis research¹⁴, we used the first 15-minute period as a benchmark from which to identify
126 within-match changes in our outcome measures. Whilst the use of this initial 15-min period as a

127 reference point from which to draw conclusions regarding fatigue from time-motion analysis metrics
128 has been questioned, due to the frantic nature of the opening exchanges in soccer ²³; we adopted this
129 analytical technique to identify within-match patterns of tri-axial accelerometer data and to make
130 inferences in regards to locomotor efficiency, rather than fatigue *per se*.

131 .

132

133 The MinimaxX S4 (Catapult Innovations, Scoresby, Victoria) contains a tri-axial piezoelectric linear
134 accelerometer (Kionix: KXP94) sampling at a frequency of 100 Hz, as part of an inertial sensor suite
135 in the micromechanical system. The output of the accelerometer measures $\pm 13g$, with each device
136 containing its own microprocessor with a 1GB flash memory and USB interface in order to store and
137 download data. The device is powered by an internal lithium ion battery with 5h of life, weighing 67g
138 and is 88x50x19mm in dimension. Vector Magnitude PlayerLoadTM (PL_{VM}) and individual-component
139 planes of PlayerLoadTM (anterior-posterior PlayerLoadTM [PL_{AP}], medial-lateral PlayerLoadTM [PL_{ML}]
140 and vertical PlayerLoadTM [PL_V]) were recorded. The calculation for PL_{VM} is the square root of the
141 sum of the squared instantaneous rate of change in acceleration in each of the three vectors (x, y and z)
142 and divided by 100¹⁹. PL_{AP}, PL_{ML} and PL_V were calculated with the same equation, using only the
143 relevant axis in the equation. Expressed in arbitrary units (au), PlayerLoadTM data were recorded using
144 the Catapult software (Sprint 5.0.9.2, Catapultsports, Melbourne, Australia). Prior to the start of each
145 season units were calibrated using the manufacturers jig to comply with the manufacturers guidelines.
146 The device was orientated and placed stationary in each plane of movement and recordings were set at
147 1g for that position to reduce any bias or drift. Every four weeks calibration values were monitored.
148 All units remained within the manufacturer's calibration tolerance limits throughout the testing period.

149

150 The MEMS device (MinimaxX, S4, Firmware version- 6.88) contains a 10Hz global positioning
151 satellite (GPS) chip in order to record the time motion analysis data. Total Distance Covered (TDC)

152 was used as a measure of the time motion analysis data (TMA). Data were included if the number of
153 satellites exceeded 6 and a horizontal displacement of positioning (HDOP) was less than 1.5. Two
154 match files were excluded as a result. To assess the within-match patterns of PlayerLoadTM and its
155 individual planes in comparison to the locomotor activities, PL_{VM} was made relative to TDC as a
156 measure of players locomotor efficiency (PlayerLoadTM per metre covered; PL:TDC).

157

158 Prior to the analysis, both Q-Q plots and stem and leaf charts were monitored to check for normal
159 distribution. Assumptions of normality were further assessed by plotting boxplots of the residuals and
160 a scatterplot of the predicted values. A linear mixed model was then used to assess the differences of
161 PL_{VM}: TDC, PL_{VM}, PL_{AP}, PL_{ML}, PL_V and TDC, between each 15-min match period. Linear mixed
162 models were able to account for the different samples between teams. Post-hoc pairwise comparisons,
163 with Sidak adjusted p values, were conducted in the event of a statistically significant F-ratio. A spline
164 model was then fitted to assess the relative change of the aforementioned variables across the first and
165 second half. For all players included in the study, an individual coefficient of variation (CV) was
166 calculated for each outcome variable, by dividing standard deviation (SD) by the individual mean from
167 each game. To explain the variance within the model playing positions, individual player and each
168 competitive fixture were included as random factors within the linear mixed model. The team for
169 which the player represented was also encompassed in the model to account for any variation in
170 tactical or physical approaches to match-play, however no effect was observed (data not shown).
171 Analyses were completed using IBM SPSS Statistics for windows software (release 20; SPSS Inc.,
172 Chicago, IL, USA) and all values are reported as mean \pm SD. Two-tailed statistical significance was
173 accepted as $p \leq 0.05$ and measures of effect size were calculated using partial eta-squared (η^2).
174 Magnitude of the effect sizes were small (>0.02), medium (>0.13) and large (>0.26)²⁵.

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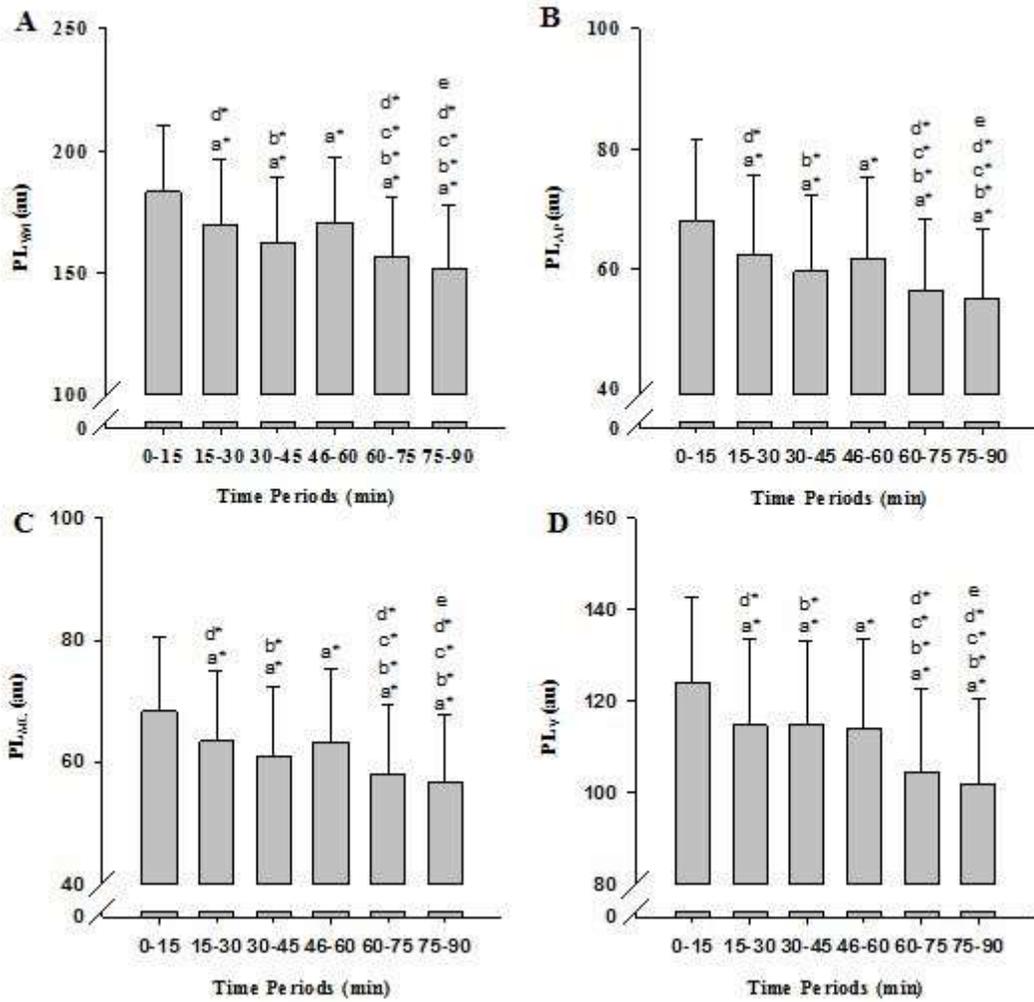
176

177 **Results**

178 The initial 0-15 mins of match play incurred a significantly higher PL_{VM} ($\eta^2=0.36-0.43$), PL_{AP}
179 ($\eta^2=0.25-0.38$), PL_{ML} ($\eta^2=0.22-0.38$) and PL_V ($\eta^2=0.29-0.42$) in comparison to all other time periods
180 (See Figure 1). During the second half, the absolute accelerometer indices progressively decreased in
181 successive 15 min match periods (see Figure 1), whereas there were no within-match changes in the
182 relative contributions (%) of each accelerometer plane.

183

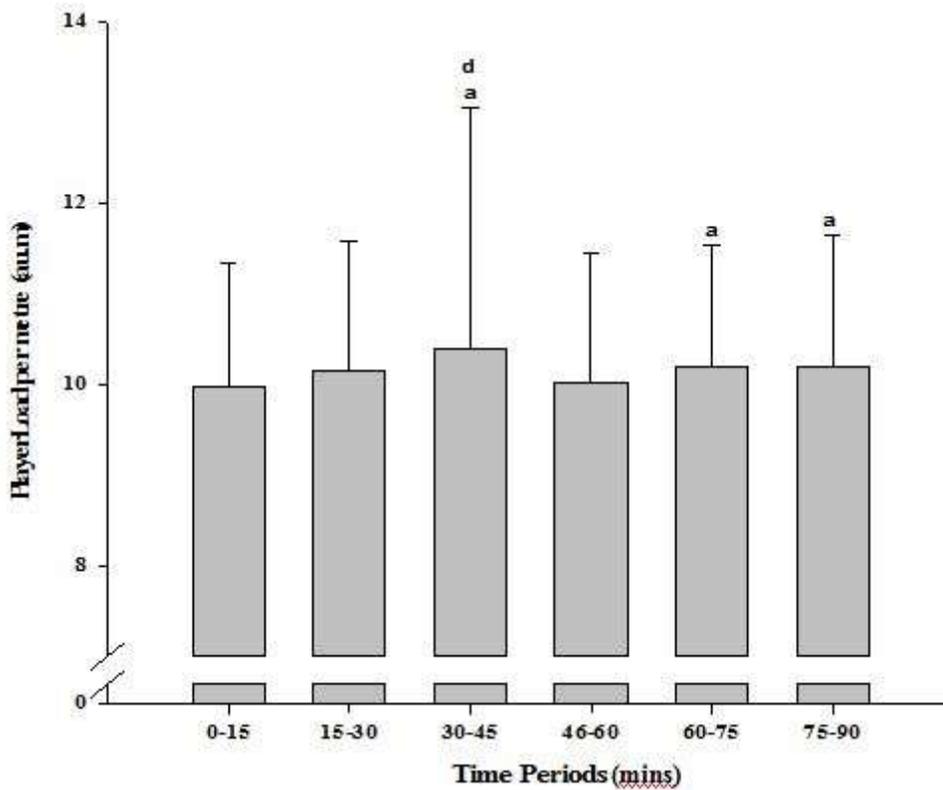
184 TDC showed significant decreases in each 15 min phase in comparison to the initial 0-15 min period
185 (0-15: 1788 ± 252 ; 75-90: 1516 ± 224 ; $\eta^2= 0.35$, $p=0.001$). TDC showed similar significant changes
186 across 15 min time periods during match play as was observed for PL_{VM} . Significant increases were
187 observed for PL:TDC towards the end of each half (See **Figure 2**; $\eta^2= 0.11-0.29$). The rate of increase
188 for PL: TDC was significantly greater in the first half (0.14 ± 0.02 au) compared to the second half
189 (0.06 ± 0.3 au; $p = 0.04$).



190

191 **Figure 1. The within-match changes in 15 min match segments for A) PL_{VM}; B) PL_{AP}; C) PL_{ML};**
 192 **D) PL_V during soccer match play. Dashed line represents 15min half-time period. ^a = difference**
 193 **versus 0-15 min; ^b difference versus 15-30 min; ^c difference versus 30-45 min; ^d difference versus**
 194 **45-60 min; * denotes a significant difference of $p \leq 0.01$. PL_{VM}- PlayerLoad™ vector magnitude;**
 195 **PL_{AP}- PlayerLoad™ in the anterior-posterior plane; PL_{ML}- PlayerLoad™ in the medial-lateral**
 196 **plane; PL_V- PlayerLoad™ vertical plane.**

197



198

199 **Figure 2. The within-match patterns of PL: TDC during soccer match play. Dashed line**
 200 **represents 15min half-time period. a- is significantly greater than the 0-15 mins, d- is**
 201 **significantly greater than the 46-60 mins. * denotes a significant difference of $p \leq 0.01$.**

202

203 The variance of PL_{VM} , the individual accelerometer planes and locomotor efficiency (PL: TDC) are
 204 illustrated in **Table. 1**. Significant findings were identified for both games and the individual player in
 205 the current model, however, no significant associations were found for position *per se*.

206

207

208 **Table 1. The individual coefficient of between-match variation and the contribution of the**
 209 **variance in soccer match play for PL_VM, the individual accelerometer planes, TDC, and**
 210 **locomotor efficiency.**

	Coefficient of Variation (95% CI's)	Game (%)	Player (%)	Positions (%)
PL_VM (au)	6.6 ± 2.4 (6.0 to 7.2)	21.6*	63.9*	14.1
PLAP (au)	8.8 ± 4.0 (7.4 to 10.4)	27.9*	40.5*	5.7
PLML (au)	9.0 ± 4.1 (6.9 to 11.0)	44.8*	36.8*	12.9
PLV (au)	7.3 ± 2.5 (5.7 to 8.9)	37.1*	36.6*	13.5
TDC (m)	6.6 ± 2.8 (3.5 to 9.5)	10.3	48.3*	8.4
PL_VM: TDC (au)	6.4 ± 2.9 (2.0 to 10.8)	21.0*	32.1*	3.6

211 **PL_VM- PlayerLoad Vector Magnitude; PL_{AP}- PlayerLoad Anterior-Posterior; PL_{ML}-**
 212 **PlayerLoad Medial-Lateral; PL_V- PlayerLoad Vertical; *represents significant**
 213 **determinant of variance within the linear mixed model (p ≤ 0.01).**

214

215 **Discussion**

216 The aim of the current study was to determine the within match-patterns of PlayerLoadTM and
 217 locomotor efficiency (PL:TDC) in professional soccer. Secondary aims of the study were to quantify
 218 the between-match variation and determinants of these external load metrics. The key findings from
 219 the present study included: 1) PL:TDC increased in the last 15 min of both the first and second halves
 220 in comparison to the initial 0-15 min period; 2) The spline model showed that the PL:TDC rate of
 221 increase was significantly greater in the first half compared to the second half, indicative of an

222 uncoupling between PL_{VM} and TDC; 3) Between-player (32.1-63.9%) and between-match (10.3-
223 44.8%) variability statistically explained the variance within the current model for PL:TDC, PL_{VM} , the
224 individual accelerometer planes and TDC.

225

226 Increased injury occurrence has been shown to occur towards the latter stages of each half within elite⁴
227 and elite youth⁶ players during competitive soccer match play. Soccer specific fatigue has been
228 purported to have an aetiological role in the increased injury incidence observed during these time
229 periods^{4,5,7}. Indeed simulated soccer matches have shown alterations in lower limb kinematics⁸,
230 strength^{8,9} and motor unit recruitment¹¹. Monitoring these responses during competitive soccer match
231 play is impractical and contravenes governing body regulations, hence external load indices have
232 traditionally been used to monitor fatiguing trends (TDC, HSR¹¹). However, methods utilising changes
233 in two-dimensional coordinates fail to quantify critical three-dimensional aspects of soccer match play,
234 such as tackles, impacts and changes of direction. In the current study, we utilised PlayerLoad™ to
235 assess the within match patterns of competitive match play, identifying reductions in three
236 dimensional loading in the latter stages of each half, a trend synonymous with injury incidence.

237 However, the locomotor patterns have shown strong relationships to PlayerLoad™ during soccer
238 training, with higher distances covered associated with greater loading¹⁸. Therefore, the progressive
239 reductions in loading identified in PlayerLoad™ during each half of match play likely reflects the
240 typical within match time-motion patterns of soccer match-play, which arguably represents the match
241 context²⁹, rather than fatigue *per se*. Hence, in this study we calculated a ratio of PlayerLoad™ to
242 total distance covered as a measure of locomotor efficiency, in an attempt to identify any uncoupling
243 which may be indicative of player fatigue. We observed a large increase in the PL:TDC during the last
244 15 min period of each half when benchmarked against the initial 0-15 min period. During a
245 standardised soccer simulation (SAFT⁹⁰), Barrett and colleagues²¹ showed PL_{VM} increased towards the
246 end of each half when the locomotor activities were fixed in 15 min segments. Using the same

247 simulation, Small and colleagues⁸ observed within match alterations in hip extension and knee flexion
248 during sprinting, which resulted in a decreased stride length in a temporal pattern that corroborates
249 with the decreased locomotor efficiency observed in this study, and that of injury incidence^{4, 5, 6}.

250 A fatigue-induced reduction in stride length during running may explain the locomotor efficiency
251 patterns we observed as its reciprocal increase in stride frequency and foot contacts incurs loading
252 detected by the accelerometer. Furthermore, increases in accelerometer metrics in the latter stages of
253 each half may reflect reduced pre-activation of the musculotendon unit associated with fatigue^{11,15},
254 leading to an impaired capacity to reduce the vibration amplitudes in lower-limb soft tissue (~20%;³⁰)
255 that result from ground reaction forces. However, caution has been advised when interpreting tri-axial
256 accelerometer data collected at the scapulae to assess lower limb movement strategy changes²¹. Whilst
257 this unit positioning is necessary for MEMS devices to enhance the GPS signal quality, laboratory
258 studies have indicated that the position of the unit between the scapulae accrues different magnitudes
259 and planar contributions of tri-axial accelerometer data versus its criterion positioning at the centre of
260 mass during both treadmill running²⁰ and a soccer match simulation²¹. The upper body movements of
261 the trunk are also non-uniform during the stochastic and combative nature of soccer match-play, and
262 may somewhat mask the lower limb changes in running kinematics¹⁰ and lower limb stiffness^{15,17, 30}.
263 The scapulae unit positioning during competitive soccer fixtures did not preclude us from identifying
264 modulations in locomotor efficiency, however future industry-practice using micro-sensor technology
265 positioned at the centre of mass may be warranted to determine lower limb loading, independent of
266 GPS monitoring.

267

268 Whilst this study has identified modulations in locomotor efficiency that may be used in industry-
269 practice to inform rotation policy by identifying players at an exacerbated risk of injury or to denote
270 the onset of fatigue, we recognise that further work is necessary to confirm our speculation. We also
271 acknowledge the crudity of our measure of locomotor efficiency, considering that total distance

272 covered by players does not represent the intermittent and intensity distribution of soccer and that
273 accelerometer loading rate is influenced by running speed²⁰. Furthermore, if observing locomotor
274 efficiency modulations has a role in reducing injury risk and fatigue management, real-time MEMS
275 data capture and processing are necessary, yet the accuracy of live GPS data has been questioned²⁶.
276 Accordingly, further work is required in terms of both aetiological research and technological
277 evolution to realise the potential application of tri-axial accelerometer data in professional sports.

278

279 To our knowledge, this study is the first to examine the between-match variation in PlayerLoad™
280 indices during actual soccer match play. We observed low coefficients of variation for the vector
281 magnitude ($6.4 \pm 2.4\%$) and its individual planes (7.3-9.0%), which in combination with its sound test-
282 retest²⁰, within- and between-device reliability¹⁹, suggests that PlayerLoad™ data may be useful for
283 practitioners to detect worthwhile changes in an athlete's external load or changes in locomotor
284 efficiency. Individual gait patterns have been speculated to cause the variation between-athletes PL_{VM}
285 values during incremental treadmill running²⁰ and during a controlled fixed soccer simulation²¹.
286 Consequently, we suggested that PL_{VM} and the individual planes should be treated and measured
287 within an individual-specific manner as a measure of external load, findings which were corroborated
288 in the current study as the individual player explained more variance in PL_{VM} (63.9%) versus the
289 match (21.6%) and positional role (14.1%) *per se*. Practitioners using accelerometer data on a routine
290 basis are therefore recommended to limit their analyses to within-player contrasts due to the large
291 variability observed between individuals.

292

293 **Conclusions**

294 PL: TDC, PL_{VM} and the individual component accelerometer planes demonstrated within-match
295 patterns during elite professional soccer match play. Towards the end of each half, the locomotor
296 efficiency (PL:TDC) increased, suggestive of an increase in the loading required for every given metre

297 of distance covered on the pitch. Since these within match patterns are concomitant with match-
298 induced alterations in strength, motor unit recruitment and lower-limb kinetics that have been linked
299 with fatigue and increased injury incidence, locomotor efficiency may be a useful tool to inform
300 substitutions or rotation policy in team sports. The efficacy of accelerometer metrics are further
301 supported by their low signal to noise ratio, but their large between-player variation limits
302 comparisons between individuals.

303

304 **Practical Applications**

- 305 • Locomotor efficiency, PL_{VM} and the individual component accelerometer planes detect
306 within-match patterns in soccer.
- 307 • The latter stages of each half show an increase in locomotor efficiency, a trend synonymous
308 with observations of increased injury incidence and fatigue.
- 309 • Locomotor efficiency may be a useful tool to inform substitutions or rotation policy in team
310 sports.

311

312 **Acknowledgments**

313 No source of funding was obtained for this study and the authors have no conflicts of interest to
314 declare. We would like to thank all players and clubs involved with the study.

315

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