

3 **Detection of microplastics in human lung tissue using μ FTIR spectroscopy**

4 **Abstract**

5 Airborne microplastics (MPs) have been sampled globally, and their concentration is known to
6 increase in areas of high human population and activity, especially indoors. Respiratory symptoms
7 and disease following exposure to occupational levels of MPs within industry settings have also been
8 reported. It remains to be seen whether MPs from the environment can be inhaled, deposited and
9 accumulated within the human lungs. This study analysed digested human lung tissue samples (n=13)
10 using μ FTIR spectroscopy (size limitation of 3 μ m) to detect and characterise any MPs present. In
11 total, 39 MPs were identified within 11 of the 13 lung tissue samples with an average of 1.42 ± 1.50
12 MP/g of tissue (expressed as 0.69 ± 0.84 MP/g after background subtraction adjustments). The MP
13 levels within tissue samples were significantly higher than those identified within combined
14 procedural/laboratory blanks (n=9 MPs, with a mean \pm SD of 0.53 ± 1.07 , $p=0.001$). Of the MPs
15 detected, 12 polymer types were identified with polypropylene, PP (23%), polyethylene terephthalate,
16 PET (18%) and resin (15%) the most abundant. MPs (unadjusted) were identified within all regions
17 of the lung categorised as upper (0.80 ± 0.96 MP/g), middle/lingular (0.41 ± 0.37 MP/g), and with
18 significantly higher levels detected in the lower (3.12 ± 1.30 MP/g) region compared with the upper
19 ($p=0.026$) and mid ($p=0.038$) lung regions. After subtracting blanks, these levels became 0.23 ± 0.28 ,
20 0.33 ± 0.37 and 1.65 ± 0.88 MP/g respectively. The study demonstrates the highest level of
21 contamination control and reports unadjusted values alongside different contamination adjustment
22 techniques. These results support inhalation as a route of exposure for environmental MPs, and this
23 characterisation of types and levels can now inform realistic conditions for laboratory exposure
24 experiments, with the aim of determining health impacts.

25 **Abbreviations**

- 26 LOD – limit of detection
- 27 LOQ – limit of quantitation
- 28 μ FTIR – micro Fourier Transform Infrared
- 29 MCT – mercury cadmium telluride
- 30 MP – microplastics between 1 μ m and 5 mm
- 31 NP – nanoplastics
- 32 PAN - polyacrylonitrile
- 33 PE - polyethylene
- 34 PES - polyester
- 35 PET - polyethylene terephthalate
- 36 PMMA - polymethylmethacrylate
- 37 PP – polypropylene
- 38 PS - polystyrene,
- 39 PTFE - polytetrafluoroethylene
- 40 PUR – polyurethane
- 41 PVA – polyvinyl alcohol
- 42 ROS – reactive oxygen species
- 43 SEBS - styrene-ethylene-butylene co-polymer
- 44 TPE - thermoplastic elastomer

45

46 **1. Introduction**

47 Microplastics (MPs), defined herein as plastic particles between 1 μm and 5 mm [1], are present in
48 all environmental compartments; from marine and freshwater bodies [2], to soil [3], food, drinking
49 water [4,5], and air [6–9]. For the latter, suspended MP particles have been isolated from many
50 atmospheric locations, including urbanised city centres [8,10,11], indoor households [7,9,12,13], and
51 remote outdoor regions [6]. Previous work highlights that citizens are exposed to higher
52 concentrations of MP within their homes [9], compared to outdoors, and this results in ubiquitous and
53 unavoidable human exposure [14]. Consequentially, there is an increasing concern regarding the
54 hazards associated with MP ingestion, dermal contact, and inhalation [14].

55 Synthetic fibres have previously been observed within human lung tissue samples [15], yet
56 limited studies confirm the presence of MPs within the lungs alongside chemical analysis tools, such
57 as μRaman and μFTIR spectroscopy [16]. Reliance upon observational criteria alone to distinguish
58 between MP and non-MPs, can lead to over and under-estimated MP counts, and a lack of information
59 relating to polymer or additive type [17,18]. The plausibility of MP inhalation has been highlighted
60 [19,20] and MPs with a width as small as 5 μm have been reported within air samples [10,21]. Upon
61 environmental release, plastics are exposed to oxidation, mechanical stress and biological action,
62 resulting in embrittlement and fragmentation, forming MPs, and eventually nanoplastics
63 (NPs)($<1\mu\text{m}$), as well as release into the environment in their primary form [18].

64 Historical studies report respiratory symptoms and disease at an occupational level of
65 exposure in synthetic textile, flock, and vinyl chloride workers [19], and as such, support inhalation
66 as an exposure route for MPs. However, it remains unclear whether MPs can enter and remain in the
67 lungs of the general population due to environmental exposure, rather than the chronic levels seen
68 within industry settings. MPs are designed to be robust materials, unlikely to break down within the

69 lungs [22], potentially leading to accumulation over time depending on aerodynamic diameter and
70 respiratory defences [19].

71 The mounting concern surrounding airborne MPs stems from the unknown polymer types,
72 levels of exposure, and consequences of their inhalation. MP characteristics such as size, shape,
73 vectored absorbed pollutants and pathogens, as well as plastic monomer or additive leaching, have
74 been highlighted as potential promoters of cytotoxicity [20]. MPs are consistently identified within
75 air samples, their concentration is highest indoors [7,12,13] and within highly populated areas [8],
76 they are readily suspended at times of high human activity [13] and are often small and fibrous [11].
77 Together, these concerns highlight the necessity for accurate tissue analysis to understand the
78 potential for these synthetic polymers to penetrate the human respiratory system and cause harm.

79 This study aims to identify any MP particles present in digested human lung tissue samples,
80 while also accounting for procedural and laboratory blank contamination. Any particles isolated from
81 lung tissue have been chemically characterised using μ FTIR spectroscopy (with a 3 μ m lower size
82 limit of detection).

83

84 2. Material and Methods

85 2.1 Human tissue acquisition

86 Excess human lung tissue was collected from thoracic surgical procedures at Castle Hill
87 Hospital, Hull University Teaching Hospitals NHS Trust, following NHS Research Ethics Committee
88 and Health Research Authority approval (REC reference 12/SC/0474). Samples of peripheral human
89 lung tissue were collected from upper, middle (left lingula) or lower lobe specimens following
90 surgical resection for cancer or lung volume reduction surgery. Descriptions of the tissue origin were
91 provided by the surgical team. Care was taken to avoid the tumour margins. Details of the donors
92 smoking status, occupation and area of residence were unavailable for the researchers under the terms

93 of the ethical approval obtained. Tissue samples were placed into empty glass containers with foil
94 lids and immediately frozen (-80°C) until bulk analysis (two batches) was conducted. Lung tissue
95 was obtained from 11 patients (numbered 1.1 to 11.1), with patients 1 and 2 providing two samples
96 (numbered 1.2 and 2.2) from different lung positions (n=13, total tissue mass=55.41 g), resulting in
97 a mean mass of 4.26±3.87 g (range 0.79-13.33 g). Patients mean age was 63±13 years (range 32-77),
98 5 females and 6 males (Table 1).

99

100 *2.2 Lung tissue digestion and filtration*

101 Thawed samples were exposed to a hydrogen peroxide (100 mL of 30% H₂O₂) bath and rinsed
102 alongside ‘procedural blanks’ (n=4) (Supplementary Fig. S1). Each tissue sample was transferred to
103 a clean glass conical flask with a foil covering, and 100 mL of 30% H₂O₂ added. The total mass of
104 each individual tissue sample digested is detailed in Table 1. Flasks were placed in a shaking
105 incubator at 55°C for approximately 11 days, 65 rpm, or until there was no visible tissue. After 5 days
106 within the incubator, an additional 100 mL of 30% H₂O₂ was added. The digest, adapted from
107 previous studies investigating MPs within different environmental and tissue samples [23], ensures
108 removal of organic particles whilst maintaining MP integrity [6,23]. Samples were then filtered onto
109 aluminium oxide filters (0.02 µm Anodisc, Watford, U.K.) using a glass vacuum filtration system.
110 These were stored in clean glass petri dishes, in the dark, before chemical composition analysis
111 alongside laboratory blanks (n=13) (Supplementary Fig. S1).

112

113 *2.3 Chemical characterisation of particles using µFTIR analysis*

114 Each tissue sample Anodisc filter was placed directly onto the µFTIR spectroscopy platform,
115 and the length (largest side) and width (second largest side) recorded using the aperture height, width
116 and angle size selection tool, available within the ThermoScientific Omnic Picta Nicolet iN10

117 microscopy software. Particles were then assigned to a shape category (fibre, film, fragment, foam,
118 or sphere [24]), whereby fibrous particles were characterised as having a length to width ratio >3
119 [12].

120 μ FTIR spectroscopy analysis was conducted in liquid nitrogen cooled transmission mode
121 (Nicolet iN10, ThermoFisher, Waltham MA, U.S.A), without the aid of further accessories or
122 crystals. The cooled mercury cadmium telluride (MCT) detector allowed for the analysis of particles
123 accurately down to 3 μ m in size. No observational criteria [18] was applied to select specific particles
124 for μ FTIR analysis, to prevent bias. Using the aperture size selection tool, all particles upon the
125 sample filter >3 μ m were included in the analysis process. For this study, the whole filter, containing
126 the total digested tissue sample, was analysed.

127 A background reference spectrum was first recorded, using identical parameters to the
128 particles undergoing analysis. A blank area of the Anodisc filter was chosen as the site for background
129 collection before immediate analysis of the sample particles. μ FTIR parameters were; spectral range
130 of 4000-1250 cm^{-1} , high spectral resolution 4 cm^{-1} , scan number of 64. No smoothing, baseline
131 correction or data transformation was attempted. Resulting sample spectra were compared to a
132 combination of polymer libraries (Omic Picta, Omnic Polymer Libraries), available with the Omnic
133 Picta software, and full spectral ranges were used with a match threshold of $\geq 70\%$. If particles were
134 below the $\geq 70\%$ match index threshold, three attempts were made to collect a successful match before
135 moving on to the next particle undergoing analysis. Particles below $\geq 70\%$ match, and particles not
136 classified as a plastic were recorded but not included in the results presented [25].

137 During μ FTIR analysis, one 'laboratory blank' Anodisc filter was opened alongside every
138 sample filter (Supplementary Fig. S1). A total of 13 lung tissue samples were analysed, plus 4
139 'procedural blanks', and 13 'laboratory blanks'. The total number of particles (MPs and others)
140 identified was 296, whereby 225 (76%) of these were above the 70% hit quality index threshold.
141 Only the MPs data is shown in the results. Identified PET and PES MP particles were reported

142 separately within this study, using a high match (>70 %) on a polymer database search to confirm
143 their identities.

144

145 *2.4 Quality assurance and control measures to reduce and quantify background MP contamination*

146 Strict control measures were adhered to, in order to quantify and characterise the nature of any
147 unavoidable background contamination. Due to the ubiquitous nature of MPs in the air, contamination
148 upon the surface of lung tissue samples could be possible during the surgical procedure, where lung
149 tissue was removed from live human subjects. While it was not possible to fully control the surgical
150 environment, each tissue sample was dropped into a 100 mL 30% H₂O₂ bath, re-sealed with foil and
151 agitated for 2 minutes. In parallel, ‘procedural blanks’ (n=4) were initiated. The tissue sample was
152 removed, and the outer surface rinsed thoroughly with 100 mL 30% H₂O₂ to remove any surface
153 contamination, employing a method similar to extracting microplastics from whole biota [26].
154 Analysis of solely the interior portion of the tissue was considered [15] but was not applied with the
155 aim of maintaining a larger tissue mass. Tissue samples were digested in two batches, with two
156 procedural blanks, which mimicked the entire tissue processing steps but lacked the lung tissue
157 sample, alongside each batch (Supplementary Fig. S1). Reagents were filtered and prepared in bulk
158 for each batch. When conducting μ FTIR analyses, a ‘laboratory blank’ filter (n=13), placed in a glass
159 sealed petri dish, was opened for the same duration as that for the tissue sample.

160 MPs found within ‘procedural blanks’ represent contamination from the laboratory reagents,
161 equipment or fallout from the air during the transfer of samples. For each batch, the average
162 procedural contamination was calculated and assumed to be present within each of the tissue samples.
163 MPs within ‘laboratory blanks’ represent contamination from atmospheric fallout within the μ FTIR
164 laboratory room during particle characterisation. Procedural blank and laboratory blank results were
165 combined to account for contamination at every step. No standardised protocols are currently adopted
166 within the MPs research field to account for background contamination, so multiple contamination

167 adjustments were applied in this study for comparison. These comprised two approaches: subtraction,
168 routinely used in the MP research field, and a limit of detection (LOD) and limit of quantification
169 (LOQ) technique [27] (Supplementary methods 1). Presenting raw data, subtraction, and LOD/LOQ
170 adjusted results allows a comparison for each technique.

171 All H₂O₂ and MilliQ water used were triple filtered using an all-glass vacuum filtration kit
172 and 47 mm glass fibre grade 6 filters (GE Healthcare Life Sciences, Marlborough MA, U.S.A). All
173 glassware underwent thorough manual cleaning, before a dishwasher cycle using distilled water and
174 then a manual three rinse wash with triple filtered MilliQ water. All equipment and reagents were
175 always covered with foil lids and a small opening made when pouring. Additionally, when filtering
176 digested samples, glassware and the sides of the filtration kit were rinsed three times with triple
177 filtered MilliQ water to avoid sample particle loss. All work was conducted in a thoroughly cleaned
178 fume cupboard with power 'off' and shield down to minimise unfiltered air flow [28] and particle
179 suspension [29]. Each tissue sample was processed individually to prevent cross contamination.
180 Plastic equipment was avoided, glass petri dishes, a cotton laboratory coat, and a new set of nitrile
181 gloves for each sample processing step. Tissue preparation and particle analysis was conducted at
182 times of low activity, no room ventilation and μ FTIR conducted in a single person room with no
183 windows. Finally, work was conducted by a single researcher for standardisation. To ensure no
184 particles were contaminating the Anodisc filters from the manufacturing process of the discs used,
185 three random filters were chosen and observed under the μ FTIR, in which no particles were present.

186

187 *2.5 Statistical analysis*

188 Tests for homogeneity and significance were performed on unadjusted MP values using SPSS.
189 All data were determined not normally distributed with a Shapiro-Wilk test and either a Kruskal-
190 Wallis or Mann-Whitney U test applied.

191

192 **3. Results**

193 *3.1 MP abundance levels detected in human lung tissue samples*

194 A total of 39 MPs were identified within 11 of the 13 human lung tissue samples. An overall
195 unadjusted mean of 3.00 ± 2.55 MPs per sample (range 0-8 MPs) were identified within human lung
196 tissue samples, significantly higher levels ($p=0.001$) compared with 0.53 ± 1.07 MP per sample
197 detected in the combined blanks. When considering the mass of the tissue sample, without accounting
198 for background contamination, a mean of 1.42 ± 1.50 MP/g was detected (Table 1). After subtracting
199 background contamination, this value becomes 0.69 ± 0.84 MP/g (Table 1). An unadjusted mean of
200 2.09 ± 1.54 MP/g of tissue was identified in male ($n=6$) and 0.36 ± 0.50 MP/g of tissue in female ($n=5$)
201 samples (adjusted to 0.91 ± 0.95 MP/g and 0.33 ± 0.52 MP/g respectively after subtracting background
202 contamination). All male samples contained at least one MP particle, whilst two of the five female
203 samples did not. The data was not normally distributed ($p=0.013$), and a Mann-Whitney U test
204 revealed tissue samples from male patients had significantly higher levels of MP/g compared to
205 females ($p=0.019$). A detailed description of the characterisation of background MP contamination
206 (procedural and laboratory blanks) can be found in the supplemental information (Table S1).

207 *3.2 MP particle characterisation from human lung tissue samples*

208 A total of 12 polymer types were identified in the tissue samples, as detailed in Fig 1 A. PP
209 (9, 23%) and PET (7, 18%) were the most abundant (Fig 1A). All MPs identified within tissue
210 samples were fibre (19, 49%), fragment (17, 43%), or film (3, 8%), (Fig 1B, Fig 2). MP particles
211 identified within the tissue samples had a mean particle length of 223.10 ± 436.16 μm (range 12-2475
212 μm), and a mean particle width of 22.21 ± 20.32 μm (range 4-88 μm) (Fig 3A).

213

214 *3.3 Characterisation of background MP contamination (procedural and laboratory blanks)*

215 Considering all the blank samples, the mean background MP contamination rate detected was
216 0.53 ± 1.07 MP per blank. Particles identified within ‘procedural blanks’ had a mean MP
217 contamination rate of 2.00 ± 2.83 MP per sample (range 0-4), for batch 1, whereby four MPs were
218 identified on one filter: PE, PE/PP, PS, and a resin particle. No MPs were detected on the second
219 filter for batch 1 (Table S1). No particles were identified within ‘procedural blanks’ from batch 2 of
220 tissue samples on either of the two procedural blank filters (Table S1). Particles detected from
221 ‘laboratory blanks’ (n=13) had an overall mean MP contamination rate of 0.38 ± 0.65 MP per sample
222 (range 0-2). This comprised one PET, PP, PS, PTFE and PVA particle from the 13 laboratory control
223 filters (Table S1). The average length of MPs detected within the combined blank samples was
224 105.22 ± 92.82 μm (range 23-315 μm), and an average width of 34.44 ± 22.61 μm (range 15-73 μm).
225 The shapes of MPs identified in the combined blank samples were either fragment (6, 67%), fibre (2,
226 22%), or film (1, 11%).

227 In addition to MP particles, non-MP ‘natural polymer’ particles were detected on the sample
228 filters. Combining non-MP procedural and laboratory blank results 9.04 ± 4.84 non-MP particles per
229 sample were detected, comprised of cellulose and zein.

230

231 *3.4 Background MP contamination adjustments*

232 Using adjustments, to account for the combined procedural and blank contamination levels
233 detected, decreases the level of MPs identified within tissue samples depending on the approach used
234 (Table 1). After blank subtraction adjustments, the total MPs identified within tissue samples have a
235 mean of 0.69 ± 0.84 MP/g of tissue. Subtraction adjusted MP levels in human lung tissues were
236 statistically significant compared to blank data (Mann-Whitney U test, $p=0.043$). Only one lung tissue
237 sample (sample 1.1) fit the criteria for using a LOD and LOQ calculation, showing 1.94 MP/g, above
238 the quantification threshold. The polymer type detected above this threshold was PP. MPs above the

239 LOD, that can be detected within lung tissue samples, but not quantified, were PE, PET, PP, PTFE
240 and resin.

241

242 *3.5 MP distribution within human samples by lung region*

243 MPs were identified within all regions of the lung (Fig 4 and Table S2). An unadjusted mean
244 of 0.80 ± 0.96 MP/g was identified within the upper region (adjusted to 0.23 ± 0.28 MP/g after
245 background subtraction), 0.41 ± 0.37 MP/g within the middle/lingular region (adjusted to 0.33 ± 0.37
246 MP/g) and 3.12 ± 1.30 MP/g within the lower region (adjusted to 1.65 ± 0.88 MP/g). Data was not
247 normally distributed ($p=0.013$) and a Kruskal-Wallis test showed that the number of MPs in the lower
248 region were significantly higher than the middle/lingular ($p=0.038$) and the upper region ($p=0.026$).
249 Within the upper region ($n=6$, total mass= 33.66 g), 11 MPs were identified; PE (2, 18%), PET (2,
250 18%), PP (2, 18%), PES (1, 9%), PS (1, 9%), resin (1, 9%), SEBS (1, 9%), TPE (1, 9%). Within the
251 middle/lingular region ($n=3$, total tissue mass= 12.19 g), 7 MPs were identified; PET (2, 29%), resin
252 (2, 29%), PE (1, 14%), PMMA (1, 14%), PUR (1, 14%). Within the lower region ($n=4$, total tissue
253 mass= 9.56 g), 21 MPs were identified; PP (7, 33%), PTFE (4, 19%), PET (3, 14%), Resin (3, 14%),
254 PS (2, 10%), PAN (1, 5%), PE (1, 5%) (Fig 4).

255 *3.6 MP distribution within human lung tissue by individual patient*

256 MPs were identified in 9 of the 11 patient lung samples. Multiple samples were taken from
257 patient 1; 8 MPs in sample 1.1 and 2 MPs in sample 1.2 (Fig 5A). PP particles were identified within
258 both samples (Fig 5B). Multiple samples were also taken from patient 2; 3 MPs in sample 2.1 and 3
259 MPs in sample 2.2. PTFE particles were identified within both samples, whilst multiple polymers
260 were only identified within one patient sample (Fig 5B).

261

262

263 4. Discussion

264 This report provides compelling evidence of MPs within human lung tissue samples, using a robust,
265 best practice, background contamination regime combined with μ FTIR chemical composition
266 analysis to verify the particles present. The study also highlights the importance of including and
267 evaluating contamination adjustments within MP research, whilst providing high levels of quality
268 assurance and control.

269 In total, 39 MPs were identified within 11 of the 13 lung tissue samples, with an unadjusted
270 average of 1.42 ± 1.50 MP/g of tissue. By subtracting any MPs detected in the corresponding blanks,
271 an adjusted average of 0.69 ± 0.84 MP/g tissue sample is reported. The MP levels within tissue samples
272 were significantly higher than those identified within combined procedural/laboratory blanks. Of the
273 MPs detected, 12 polymer types were identified with PP (23%), PET (18%), resin (15%), and PE
274 (10%) the most abundant. It should be noted that the FTIR spectra for PET and PES (polyester) are
275 similar and can be difficult to distinguish [30,31], however a high match of 70% was accepted to
276 distinguish between the MP types within this study.

277 MPs were identified within all regions of the lung categorised as upper (0.80 ± 0.96 MP/g),
278 middle/lingular (0.41 ± 0.37 MP/g), and lower (3.12 ± 1.30 MP/g) region. However, when a LOD and
279 LOQ approach was applied, only one tissue sample fit the criteria, with only PP detected above the
280 threshold levels at 1.94 MP/g (Table 1). It could be that most MPs identified were contamination,
281 however the LOD LOQ could also be 'masking' legitimately identified MPs. The LOD LOQ
282 adjustment approach dramatically reduced the level of quantifiable MPs identified within lung tissue
283 samples. This quality control measure has the benefit of providing a threshold above that of a simple
284 subtraction, allowing MPs to be reliably detected and quantified [26]. Although it is an emerging
285 technique within the MP field, it has the potential to account for polymer type as well as quantity and
286 is commonly applied within analytical chemistry. However, samples containing low numbers of MPs,
287 such as the human lung tissue samples reported here, commonly only have one MP particle per

288 polymer type identified in a sample. It has been reported that when dealing with such low MP
289 quantities within samples, the LOD LOQ technique will have more significant effects and lead to a
290 “reduced capacity to report any MPs above the LOD or LOQ” [27]. We therefore report our results
291 in three ways; unadjusted, subtraction adjusted and LOD LOQ adjusted, but highlight the importance
292 of the LOD LOQ technique for future studies in which MP abundance is not as low.

293 MPs have, to date, been detected in human samples from histological lung cancer samples
294 [15] and cadavers [16] as well as from human placenta [32]. Our findings are consistent with an early
295 study by Pauly et al (1998) using microscopy under polarised light to identify fibres (though without
296 chemical characterisation validation or rigorous contamination control measures), reporting presence
297 of fibres in 83% of nonneoplastic lung specimens (n=67/81) and in 97% of malignant lung specimens
298 (n=32/33)[15]. This study also reported that the fibres were distributed throughout all regions of the
299 lung and were not confined to the large air spaces [15]. While no formal size range is given in this
300 early study, they reported heterogeneity with respect to fibre length, width, surface morphology and
301 colour, with >250 µm length and ~50 µm width [15]. Our findings are also in line with a recent
302 publication by Amato-Lourenco *et al* who also found PP to be amongst the most abundant plastics
303 identified [16]. In contrast to our study, Amato-Lourenco *et al* showed that non-fibrous particles
304 were the most abundant type of MP with sizes smaller than those seen in our study. This could partly
305 be due to differing exposures to MP, our best practice approach used to eliminate background
306 contamination, or the methods used to detect and characterise samples, Raman vs. µFTIR. Although
307 Raman spectroscopy has the advantage of a lower method detection limit (~1µm), which might
308 explain the abundance of smaller particles identified in Amato-Lourenco’s study [16], it can be
309 heavily influenced by fluorescence interference and does not detect the same polar peaks that µFTIR
310 spectroscopy can. Additionally, Raman spectroscopy can UV degrade the particles being analysed,
311 which could hinder potential future investigations. Thus, although both spectroscopic techniques
312 complement each other, µFTIR has some advantages that benefit MP research [33].

313 Interestingly, tissue from male donors contained significantly higher levels of unadjusted MP
314 (2.09 ± 1.54 MP/g) compared to females (0.36 ± 0.50 MP/g), with all samples from males containing
315 MPs but two out of five samples from females showing no MPs. We hypothesise that this is due
316 female airways being significantly smaller than the airways of males [34], although the relatively
317 small sample size used herein dictates that more analyses be conducted to explore such differences
318 further.

319 According to Donaldson et al (1993), only particles with a physical diameter smaller than 3
320 μm can enter the alveolar region of the lung [35]. The alveolar duct is reported in the literature as
321 being ~ 540 μm diameter and 1410 μm long [36]. Particles of a size ranging from 12-2,475 μm for
322 length and 4-88 μm for width were detected within lung samples in this study, in theory, too large to
323 be present, yet present nonetheless.

324 While the fate of particles entering the lung, and their resulting biological effects in terms of
325 inflammation responses, are well established for ultrafine particulates in the NP or PM_{10} size range
326 [37,38], the corresponding information is currently unavailable for the MP size range of particles
327 observed here, highlighting a serious gap in the knowledge. There are limited recent studies giving
328 evidence of particle sizes and deposition in the lungs. It could be that there may be a pre-conceived
329 assumption about the particle sizes which are inhalable and able to make it into the lower airway, but
330 in this study, and others [15, 16] particles bigger than these are being reported, and therefore, it may
331 be time to revisit these numbers and investigate what sizes can be inhaled. Interestingly, even after
332 LOD and LOQ were applied, the PP identified in sample 1.1 were all above the size limit which is
333 generally thought of as inhalable.

334 12 MPs ≤ 10 μm were identified within 7 of the 13 lung tissue samples, consisting of PET (3),
335 resin (3), PE (2), PP (2), PTFE (1) and PAN (1) (Table 1). The smallest particle identified was 14 μm
336 in length and 4 μm width (Fig. 2C), and identified as an 'alkyd resin', a synthetic thermoplastic used
337 in protective coatings and paints [39]. No MPs ≤ 10 μm were detected within blanks, surprising since

338 the prevalence of MPs in the environment is known to increase with decreasing particle size [6–8],
339 suggesting that the quality assurance measures undertaken eliminated these smaller particles from
340 blanks. As these small MPs were consistently absent from blanks (Fig. 3B), it highlights the
341 likelihood of the smaller MPs being present within lung tissue rather than from background
342 contamination sources.

343 The ubiquity of MPs within the environment, results in background contamination in any
344 study, even after strict quality control measures are applied. Blanks, or controls, are run alongside
345 sample analysis to document the levels and types of MPs contaminating samples, either by mimicking
346 the sample processing steps ('procedural blank'), or by opening a clean filter during sample analysis
347 ('laboratory blank'). Rarely are procedural and laboratory blanks both applied [26]. It was
348 hypothesised in the design of this study that if MPs were present within lung tissue samples, they
349 would be present at low levels, especially considering the detection limit of chemical verification.
350 Thus, the importance of combining multiple procedural and laboratory blanks, is highlighted. In this
351 study the MP characteristics identified within blanks were distinct from those identified within lung
352 tissue samples; the main polymer abundance, size range and shape varied (Fig 3A, 3B). Human lung
353 tissue samples were typically comprised of PP, PET and resin, with lengths ranging from 12-2475
354 μm and widths from 4-88 μm , and fibres being more prevalent than fragments. In contrast, MPs
355 detected in the blanks were less abundant and comprised different particle characteristics. MPs were
356 sized 23-315 μm and 15-73 μm for length and width, and fragments were more prevalent than fibres.

357 Within the MP literature, a standardised contamination adjustment technique has not been
358 established. Therefore, this study opted to report concentrations in three commonly used ways;
359 detailing blank results but making no adjustments [13,40], subtraction adjustments [6,41] and LOD
360 LOQ adjustments [9,27]. Using no contamination adjustments, 1.42 ± 1.50 MP/g of lung tissue was
361 observed. While this method is common practice, it likely includes any contamination within the
362 samples. The subtraction adjustment decreases the lung tissue MP final mean value to 0.69 ± 0.84
363 MP/g and accounts for any potential background contamination but is not specific in terms of taking

364 into account particle characteristics. The LOD LOQ adjustment approach dramatically reduces the
365 levels of MPs identified within the study to 0.15 ± 0.54 MP/g using a polymer specific approach, but
366 could be seen to 'mask' low levels of MPs. Ultimately this study highlights the need for data
367 adjustments to account for background contamination, but alongside an evaluation into which
368 adjustment is the best approach. Irrespective of the adjustments, low levels of MPs are present within
369 lung tissue samples, providing evidence to support MP inhalation as a route of exposure to humans.

370 Airborne MPs are globally ubiquitous and especially prevalent indoors where humans spend
371 many hours a day, such as the home [7,9,12,13] and the office [7,13]. Humans are thus continuously
372 exposed to atmospheric MPs, with inhalation estimates ranging from 6-272 MP/day [12,19,42]. It is
373 the smallest and least dense MP and NP particles that are the most cause for concern regarding
374 respiratory health, as these MPs are most likely to deposit within the lungs based on aerodynamic
375 diameter [19]. In contrast to NPs, MP particles in the full micro-size range (10 μ m-5 mm) have yet
376 to be considered in terms of health implications and potential impacts, perhaps not having been a
377 priority compared with the smaller, ultrafine particles. The results herein indicate that the larger
378 micro-size range are detected within human lung samples, suggesting that these have been overlooked
379 (as being considered too large to enter lungs). MPs, like all macroplastics, are designed to be resilient,
380 with the addition of dyes, and additives that dictate their properties [2]. It had previously been
381 suggested that inhaled MPs are likely to bio-persist and possibly accumulate within a lung
382 environment [20], showing resilience to degradation by synthetic extracellular lung fluid after 180
383 days [22]. After deposition within the lung, mechanisms of toxicity are unknown but particle
384 properties such as small size, density, concentration, shape, monomer type, chemical leachates and
385 environmental adsorbents (e.g. bacteria, heavy metals and polyaromatic hydrocarbons) have all been
386 suggested as potential contributors to cytotoxicity [19,20]. Inflammation [43], ROS and oxidative
387 stress [44], physical damage from particle shape, frustrated phagocytosis [35], are currently suggested
388 cellular responses to MP exposure.

389 In summary, this study is the first to report MPs within human lung tissue samples, using
390 μ FTIR spectroscopy. The abundance of MPs within samples, significantly above that of blanks,
391 supports human inhalation as a route of environmental exposure. MPs with dimensions as small as 4
392 μ m but also, surprisingly, >2 mm were identified within all lung region samples, with the majority
393 being fibrous and fragmented. The knowledge that MPs are present in human lung tissues can now
394 direct future cytotoxicity research to investigate any health implications associated with MP
395 inhalation.

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503

504 **Table legend**

505 **Table 1.** Patient and tissue sample information alongside the number of MPs identified within
506 samples by μ FTIR spectroscopy. Polymer types and particle characteristics are included, and three
507 different contamination adjustments to display results in units of MP/g of tissue. Abbreviations;
508 PAN=polyacrylonitrile, PE=polyethylene, PES=polyester, PET=polyethylene terephthalate,
509 PMMA=Polymethylmethacrylate, PP=polypropylene, PS=polystyrene,
510 PTFE=polytetrafluoroethylene, PUR=polyurethane, Resin=alkyd/ epoxy/ hydrocarbon,
511 SEBS=styrene-ethylene-butylene co-polymer, TPE=thermoplastic elastomer. R=right lung, L=left
512 lung, Low=lower region of the lung, mid=middle/lingular region of the lung, up=upper region of the
513 lung

514

515 **Figure legends**

516 Fig. 1. Polymer types (A) and shapes (B) of the MPs identified within lung tissue samples.

517 Fig. 2. Images of MPs identified from human lung tissue samples. A, B, C and D= (A=PET) (B=PUR)
518 (C=Resin) (D=PAN). E and F=MPs identified within blanks. (E=PS) (F=PP). Corresponding spectra
519 included in Fig. S2.

520 Fig. 3. Polymer size dimensions and type of each MP identified within (A) human lung tissue samples
521 and (B) 'procedural blank' (triangles) and 'laboratory blank' (circles) samples. Red line represents
522 the assumed inhalable size limit regardless of density.

523 Fig. 4. Particle number (total MPs detected with no account taken for MPs found in controls) and
524 polymer type of MPs identified within human lung tissue samples, assigned to their lung region.

525 Fig. 5. Number (A) and type/quantity (B) of MPs detected in each lung region for individual patients.